



Scuola Superiore
Sant'Anna



Sant'Anna
Scuola Universitaria Superiore Pisa

Counteracting balance loss by using wearable robotics

Speaker: Vito Monaco

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Bari, 20 May 2019

Thanks to Prof. V. Bevilacqua for the invitation

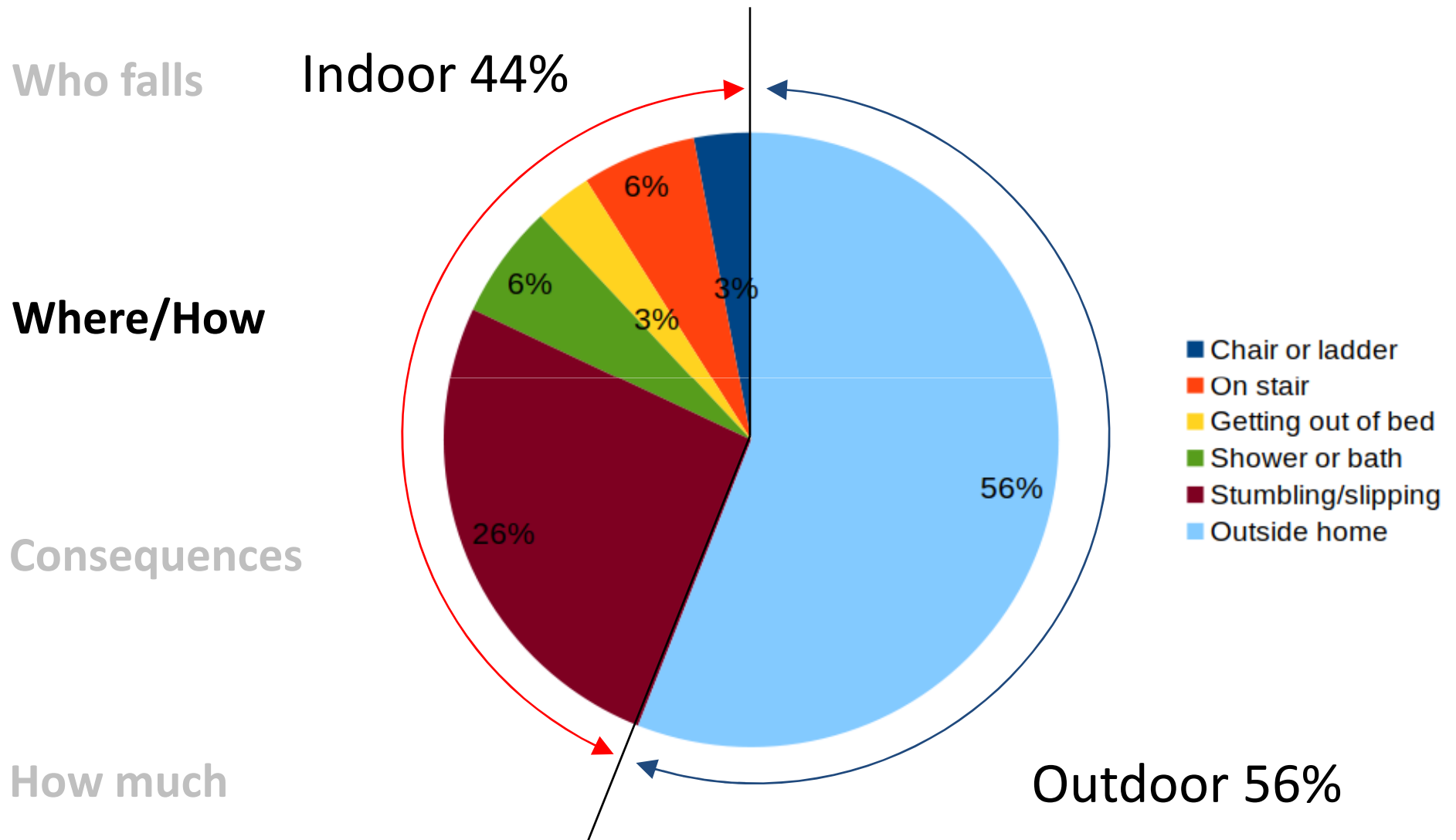
Outline of the presentation

- **Fall risk: what are we talking about?**
- State of art
 - Assessing the fall risk
 - Detecting falls/lack or balance
 - Counteracting falls/lack of balance
- Wearable robot: the dream
- Our toolbox
 - SENLY
 - Active Pelvis Orthosis
- A possible strategy
 - Detection Algorithm
 - Assistive strategy
- Ongoing activities
 - Different perturbations
 - Other approaches for the detection
 - Robotic prosthesis
- Conclusions

Fall risk: what are we talking about?

	Risk factor	Range		
Who falls	Age	+ 65	Fall risk (1 fall per year)	30%
		+ 80		50%
Where/How	Gender	M	Injury rate	F > M
		F		
	Medical Conditions	<ul style="list-style-type: none"> • Diabetes • Parkinson's disease • Depression • Incontinence • Alzheimer disease 		
Consequences	Physical Conditions	<ul style="list-style-type: none"> • Muscle weakness • Impaired balance • Gait deficits • Visual deficits 	<ul style="list-style-type: none"> • Limited mobility • Cognitive impairments • Impaired ADL • Postural Hypothension 	
How much	Behavioral factors	<ul style="list-style-type: none"> • Sedentary lifestyle • Medication intake • Alcohol misuse • Inappropriate shoes 		

Fall risk: what are we talking about?



Fall risk: what are we talking about?

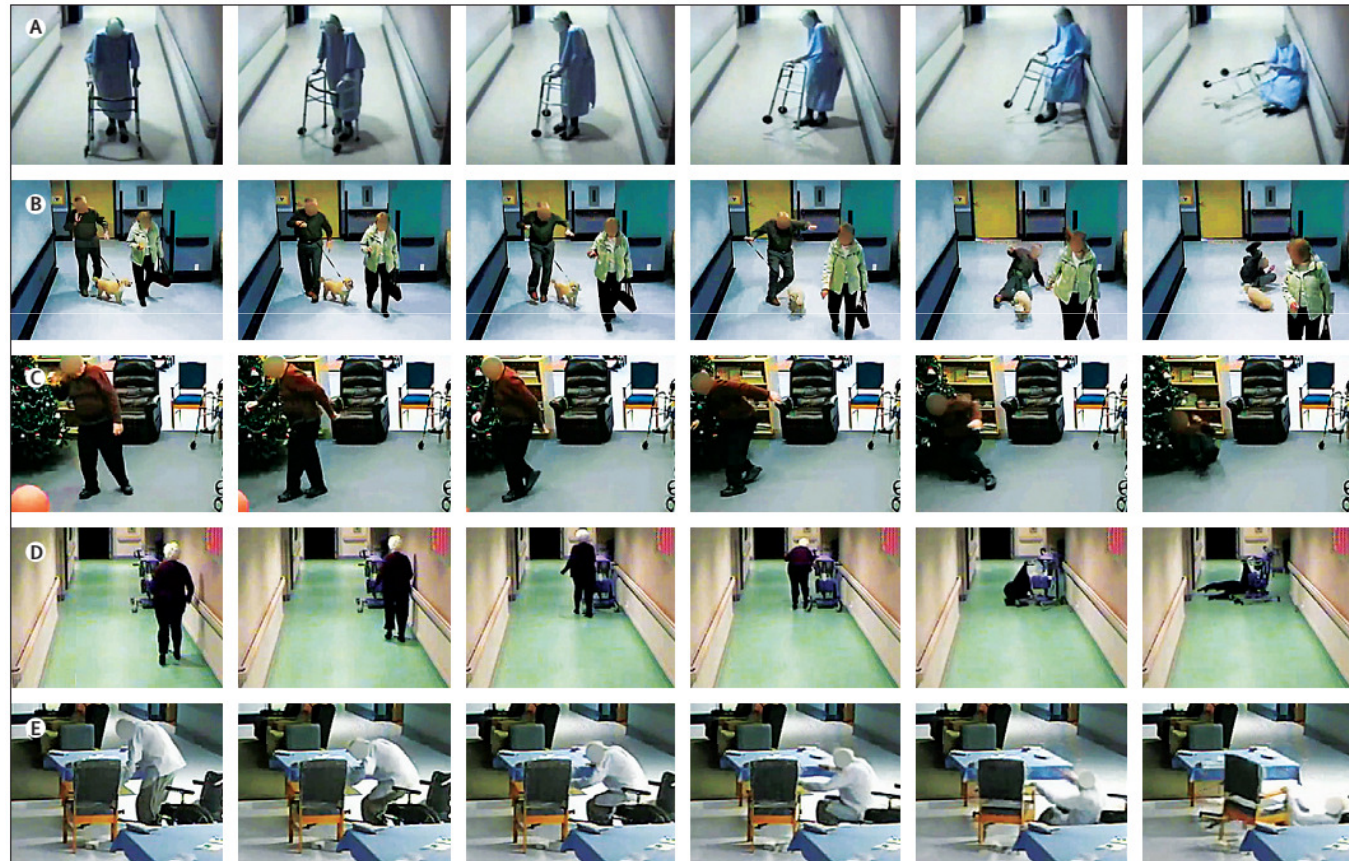
Video capture of the circumstances of falls in elderly people residing in long-term care: an observational study

Who falls

Where/How

Consequences

How much



Fall risk: what are we talking about?

Video capture of the circumstances of falls in elderly people residing in long-term care: an observational study

Who falls

Estimated proportion of participants falling at least once, and average number of falls per participant, attributable to various causes of falling

Where/How

	Frequency [*]		Participants falling due to this cause [†]		Number of falls per participant [†]	
	Number	Percentage of falls captured	Estimated proportion, % (SE)	95% CI	Estimated count, n (SE)	95% CI
Incorrect transfer or shift of bodyweight	93	41%	51.2% (4.5)	42.5–59.8	0.72 (0.078)	0.59–0.90
Trip or stumble	48	21%	26.0% (3.9)	19.1–34.3	0.35 (0.054)	0.26–0.47
Hit or bump	25	11%	17.3% (3.4)	11.7–25.0	0.19 (0.040)	0.13–0.28
Loss of support with external object	25	11%	18.9% (3.5)	13.0–26.7	0.20 (0.041)	0.13–0.30
Collapse or loss of consciousness	24	11%	16.5% (3.3)	11.0–24.1	0.17 (0.039)	0.11–0.27
Slip	6	3%	4.7% (1.9)	2.1–10.2	0.047 (0.020)	0.021–0.11
Could not tell	6	3%

In descending order of frequency.

^{*} Of 227 total falls captured.

[†] Of 215 falls analysed, after exclusion of cases for which the faller could not be identified (six), and cases for which the team could not identify the cause of the fall (six).

How much

Robinovitch et al., Lancet 2013

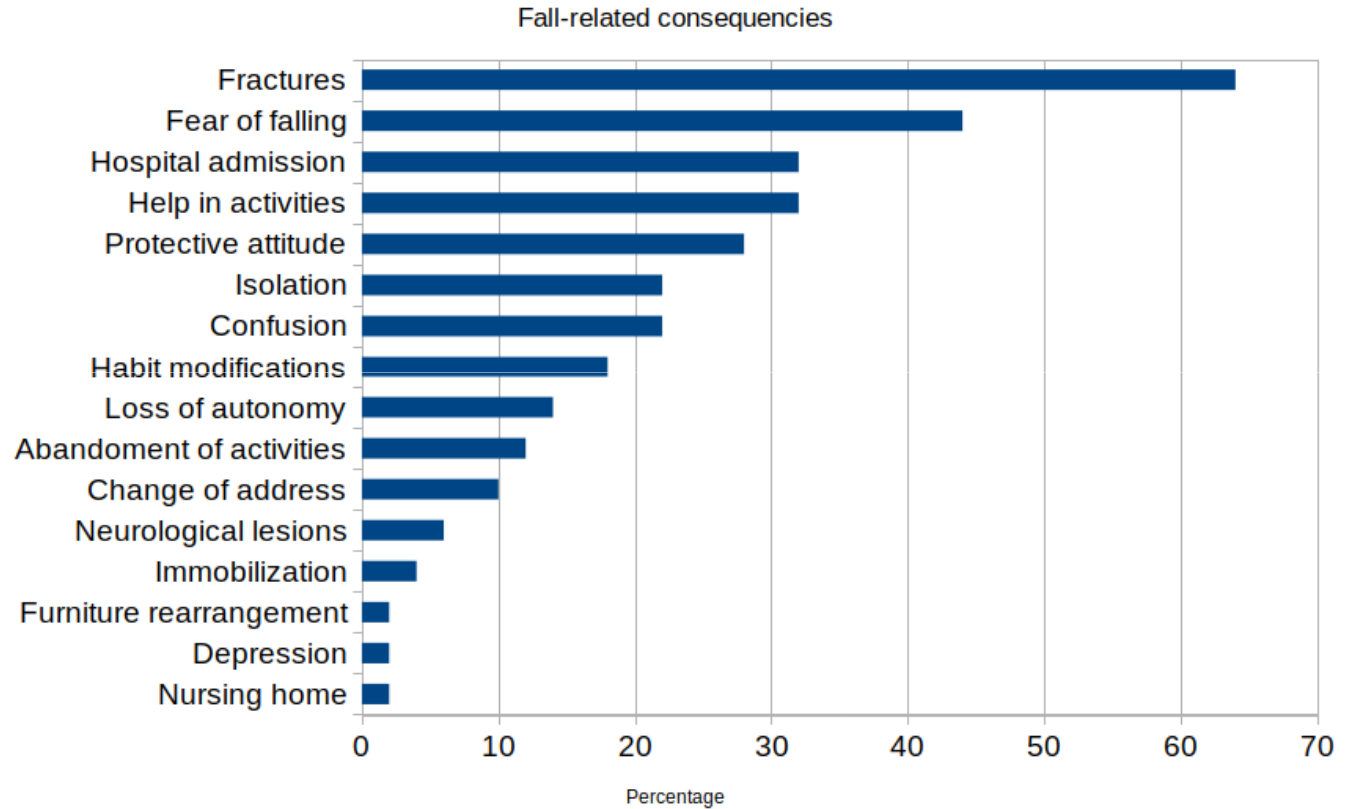
Fall risk: what are we talking about?

Who falls

Where/How

Consequences

How much



Fall risk: what are we talking about?

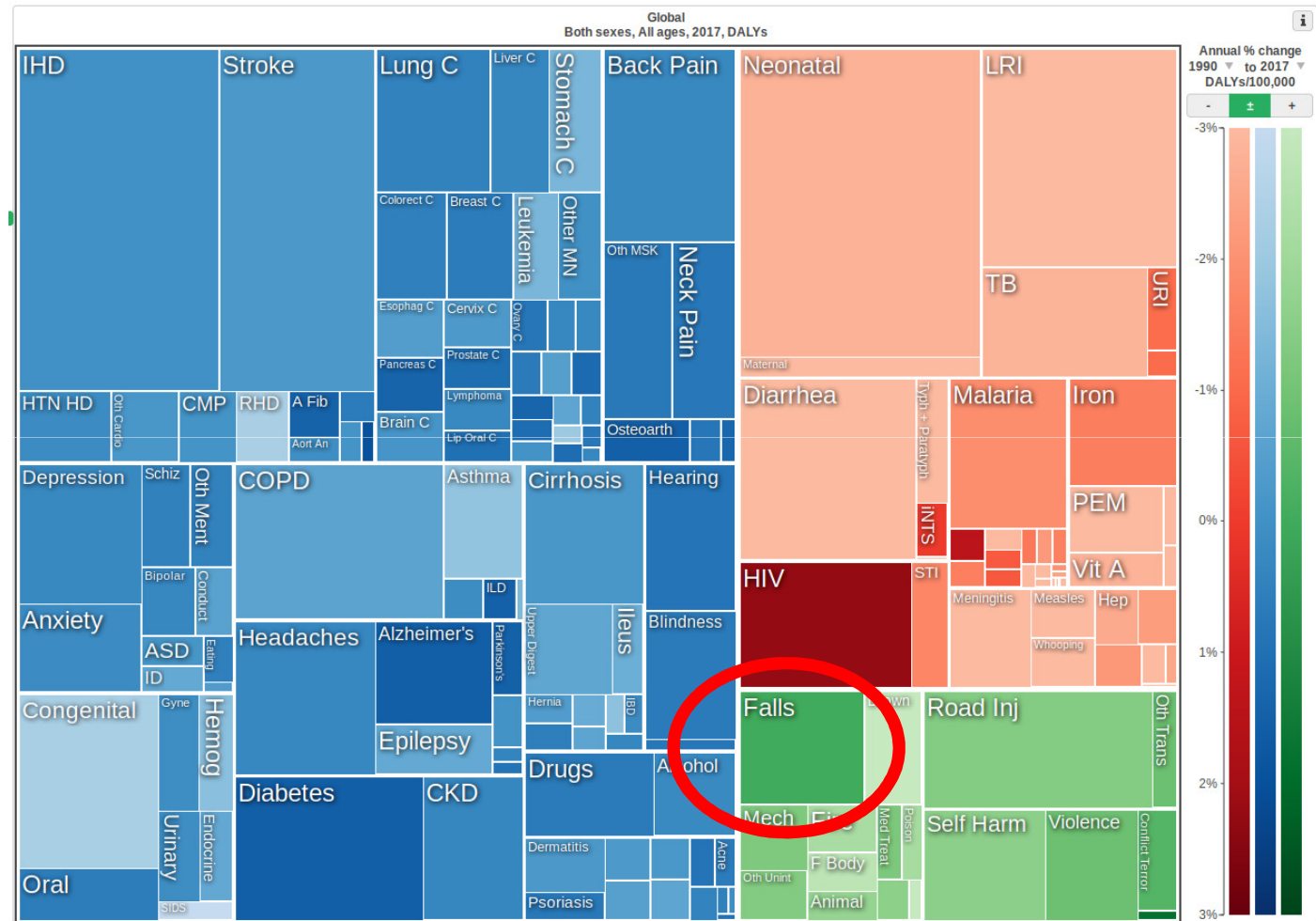
Global Burden of Disease

Who falls

Where/How

Consequences

How much



DALYs ~ the number of years lost due to the ill-health, disability, or early death

Fall risk: what are we talking about?

Who falls

- Fall-related injuries are among the most expensive health conditions
- In 2000, \$179 million were spent on fatal falls and \$19 billion were spent on injuries from non-fatal falls in US

Stevens et al., Inj. Prev. 2006

Where/How

Consequences

- Modena University Hospital 2012
 - 220/240 hip fracture per year
 - € 10.000 per fracture
 - € 2.2-2.4 million per year
- Italy: € 1 billion per year due to falls
- Europe: € 800 billion per year due to falls

How much

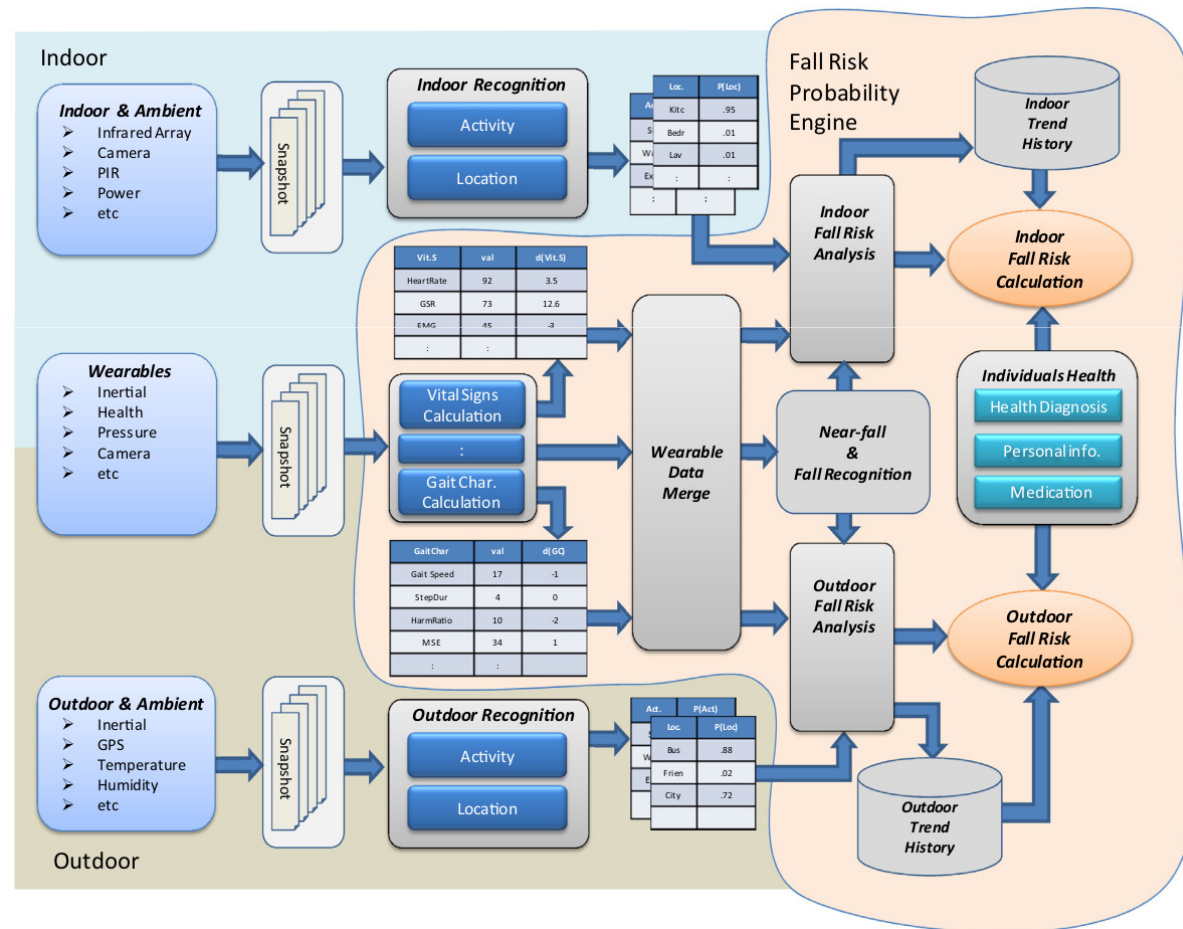
Dr. La Porta, SIAMOC 2018

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Assessing the fall risk

Fall risk assessment is a process in which the probability of a future fall is estimated, usually within a timeframe of 6–12 months.



Detecting falls

Personal Emergency Report System (PERS 2.0)

- **How it works**

- Devices able to detect a fall after it occurs in order to overcome long-lie conditions;
- Based on smart environments, video-cameras, acoustic or inertial sensors, and mobile phone technology.

- **Limits**

- Able to detect a fall only after the subject hits the ground
- Some of them only work in structured environments

- **Commercially available**

Wearable sensors



Lifeline with AutoAlert

myHalo



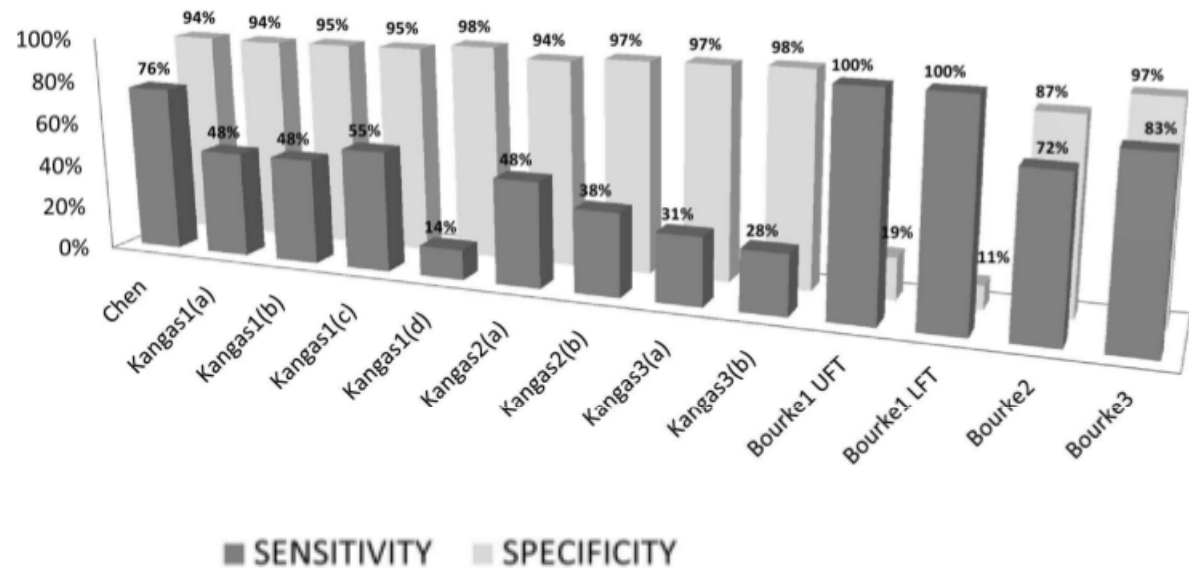
myHalo® Auto Fall Detect Pendant by MobileHelp®

Detecting falls

The screenshot displays the Google Play Store interface. At the top, the Google Play logo is on the left, followed by a search bar and a search icon. On the right, there are icons for a grid of apps and a globe. Below the search bar, a navigation bar includes 'Categories', 'Home', 'Top Charts', and 'New Releases'. A left-hand sidebar menu lists options: 'My apps', 'Shop', 'Games', 'Family', 'Editors' Choice', 'Account', 'Payment methods', 'My subscriptions', 'Redeem', 'Buy gift card', 'My wishlist', 'My Play activity', and 'Parent Guide'. The main content area is titled 'Apps' and features a grid of 14 app cards. Each card shows the app icon, name, developer, and a star rating.

App Name	Developer	Rating	Price
Fall detection	TestM	★★★★★	
Fall Detection – Fall	Deskshare, Inc	★★★★★	€3.09
mynotifi - Fall Dete	MedHab	★★★★★	
Seizarrio: Seizure an	HealthAppy Tech	★★★★★	
FallSafety Pro—Saf	Tidyware, LLC	★★★★★	
Chk-In Fall Alert	SNI	★★★★★	
Fall Detection with	FM apps & games	★★★★★	
Walabot HOME - Fe	Walabot	★★★★★	
Fall Detector	HuynhCongHuy	★★★★★	
Senior Safety App,	97 Technologies	★★★★★	
Fall Warner	Telnet	★★★★★	
LoneAlarm	LoneAlarm Pty Ltd	★★★★★	
EmergencyApp	EmergencyAppX	★★★★★	
Fall-Detect	Alexander.Morgan	★★★★★	

Detecting falls: do current algorithms work in the real world?



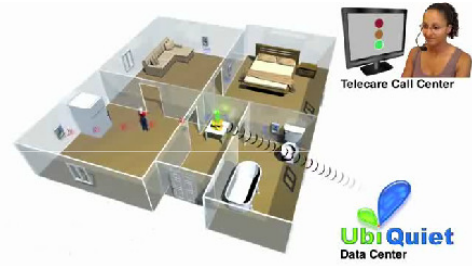

Algorithms

- tuned on simulated falls
- tested on real falls

Algorithms based on simulated data do not work very well in the real World

- **Sensitivity** measures the proportion of actual positives which are correctly identified
- **Specificity** measures the proportion of negatives which are correctly identified

Detecting falls

	Pros	Cons
Sensorized Environments  The diagram illustrates a sensorized environment. On the left, a call center is shown with several workstations, each equipped with a computer monitor and a headset. A person is visible at one of the workstations. On the right, a data center is depicted with server racks and a large blue antenna. The text 'Telecare Call Center' is positioned above the call center, and 'Ubi Quiet Data Center' is positioned below the data center. A signal wave is shown connecting the two environments.	<ul style="list-style-type: none">• Many sensors• Mitigate fall consequences (“long lie”)• Autonomous	<ul style="list-style-type: none">• Structured Environments• Invasive• Act after falling
Wearable Sensors  The image shows a person's wrist wearing a white, rectangular, wrist-worn sensor. The sensor has a small display screen and a black strap. A hand is visible, pointing towards the sensor.	<ul style="list-style-type: none">• Unstructured Environments• Embedded in personal devices	<ul style="list-style-type: none">• Not reliable set-up• Non Autonomous

Pre-impact fall detection



Lack of balance \neq fall

- Falling: lying on the ground after hitting it

- Lack of balance: maybe, you can still recovery the balance... maybe not

- Pros

- to timely ask for assistance
- to timely activate fall protection systems

- Weaknesses

- data collected in structured environments
- protection system: any suggestion?

Pre-impact fall detection

Experimental sessions



- Pros
 - to timely ask for assistance
 - to timely activate fall protection systems
- **Weaknesses**
 - **data collected in structured environments**
 - protection system: any suggestion?

Pre-impact fall detection

Protection systems

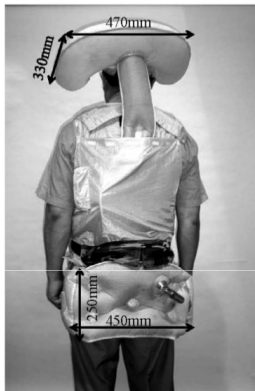


TABLE II
INFLATION TIME OF THE AIRBAG WHILE MIMICKING A FALL USING
THE PROPOSED ALGORITHM

Subjects	Inflation time	Fall time
1	0.100	0.207
2	0.140	0.387
3	0.133	0.223
4	0.121	0.177
Ave	0.121	0.249
SE	0.019	0.094

- **Pros**

- to timely ask for assistance
- to timely activate fall protection systems

- **Weaknesses**

- data collected in structured environments
- **protection system: any suggestion?**



Start to fall



Detect fall



Inflate airbag



Completely inflate



Fall

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Wearable robots: the dream



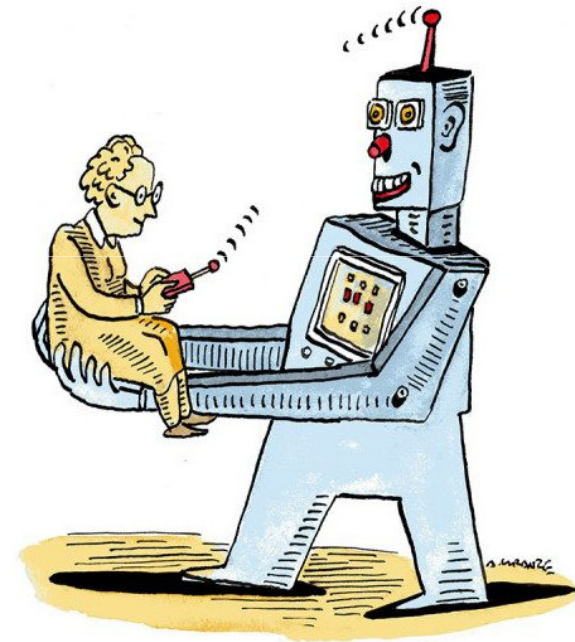
“Perhaps in the latter half of this century, exoskeletons and orthoses will be as pervasive in society as wheeled vehicles are today.”

Herr, JNER 2009

Why robots against falls?

Wearable robots are:

- equipped with sensors to monitor subjects' dynamical conditions
- equipped with actuators to modify user's dynamical balance
- controllable/programmable
- multiple purposes platforms
- active before falling
 - not hitting the ground
 - not stigmatizing the balance loss



Wearable robots: the dream



HAL5
[Cyberdyne]



Hyundai Exoskeleton
[Hyundai Motor]



Rewalk
[Argo]



Body weight support
[Honda]



HAL Lumbar for labor support
[Cyberdyne]



HAL Lumbar for care support
[Cyberdyne]

Wearable robots

What they do

Full body exoskeletons



not currently used in daily-life scenarios except for strongly motivated persons affected by severe diseases
(e.g., young patients affected by spinal cord injury resulting after a traumatic accident)

Pelvis exoskeletons



Can these be used to counteract the lack of balance?

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Our experimental setup: SENLY



Transnational access – **free of charge** –
to research infrastructures

Main features:

- size 2.5m x 2.5m
- double split treadmill
- AP belt movement
 - max speed 1.8 m/s
 - max acc 8 m/s²
- ML belt movement
 - max disp 0.3 m
 - max speed 1.25 m
 - max acc 2.4 m/s²
- Sensorized platform

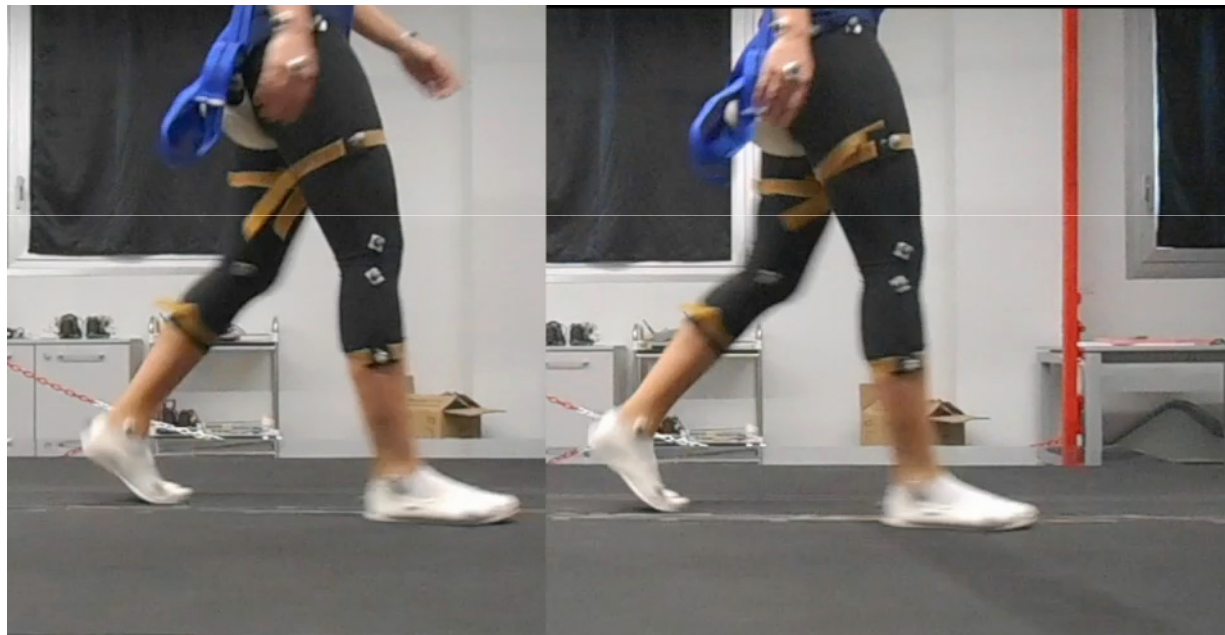
Bassi Luciani et al., JNER 2012

Modulating the intensity of the perturbation

Onset: HS of the limb being perturbed

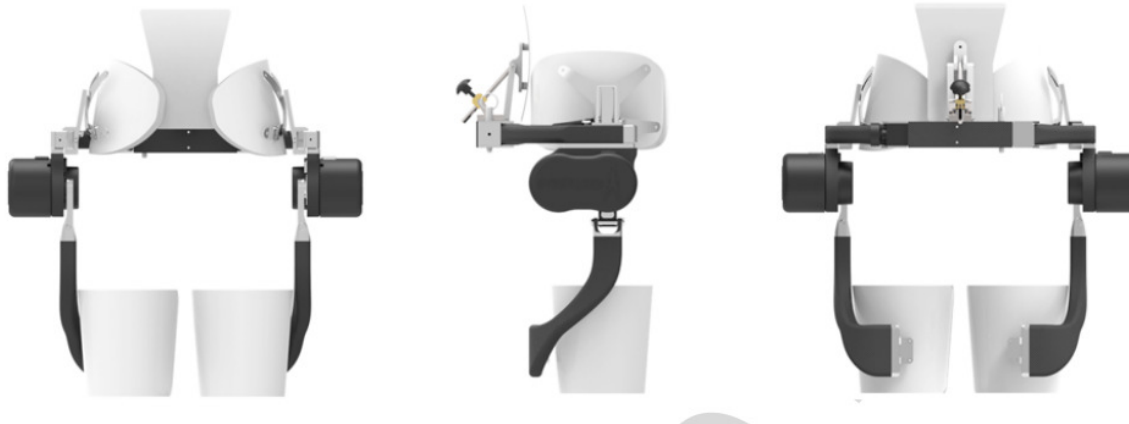
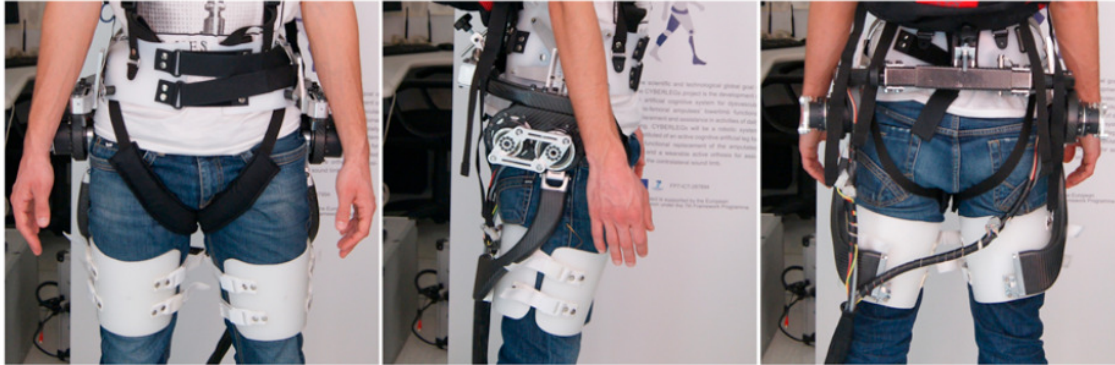
Onset: TO of the contralateral limb

HS



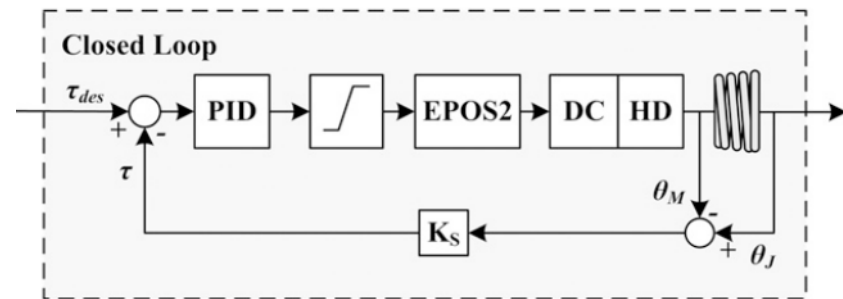
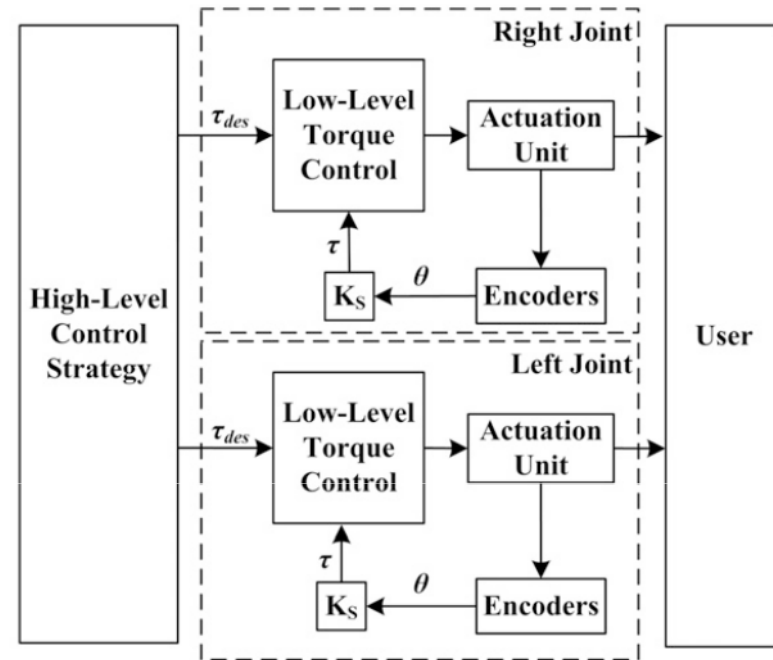
TO

Active Pelvis Orthosis (APO)



Active and Passive degrees of freedom		
Active flexion/extension RoM	Extension: -30 deg	Flexion: 110 deg
Passive abduction/adduction RoM	Adduction: -15 deg	Abduction: 45 deg
SEA Characteristics		
Motors	100 W BL DC Maxon Motor	
Reduction Stage	100:1 Harmonic Drive	
Spring Stiffness	100 Nm/rad	
SEA Performance		
Max torque	Continuous: 20 Nm	Peak: 35 Nm
Joint output mechanical impedance	< 1 Nm/rad @ 1 Hz	
Closed-loop torque-control bandwidth	15 Hz	
Control Architecture Characteristics		
Low-level controller sampling rate	1 kHz	
High-level controller sampling rate	1 kHz	
Others		
Weight	4.2 kg	
Safety limits	Active DoF out of RoM	Joint speed > 400 deg/s
Power Supply	48 V	

Active Pelvis Orthosis (APO)



Active Pelvis Orthosis (APO)

α -prototype



β -prototype

γ -prototype

SPIN  ff
Impresa Spin-Off della Scuola Sant'Anna

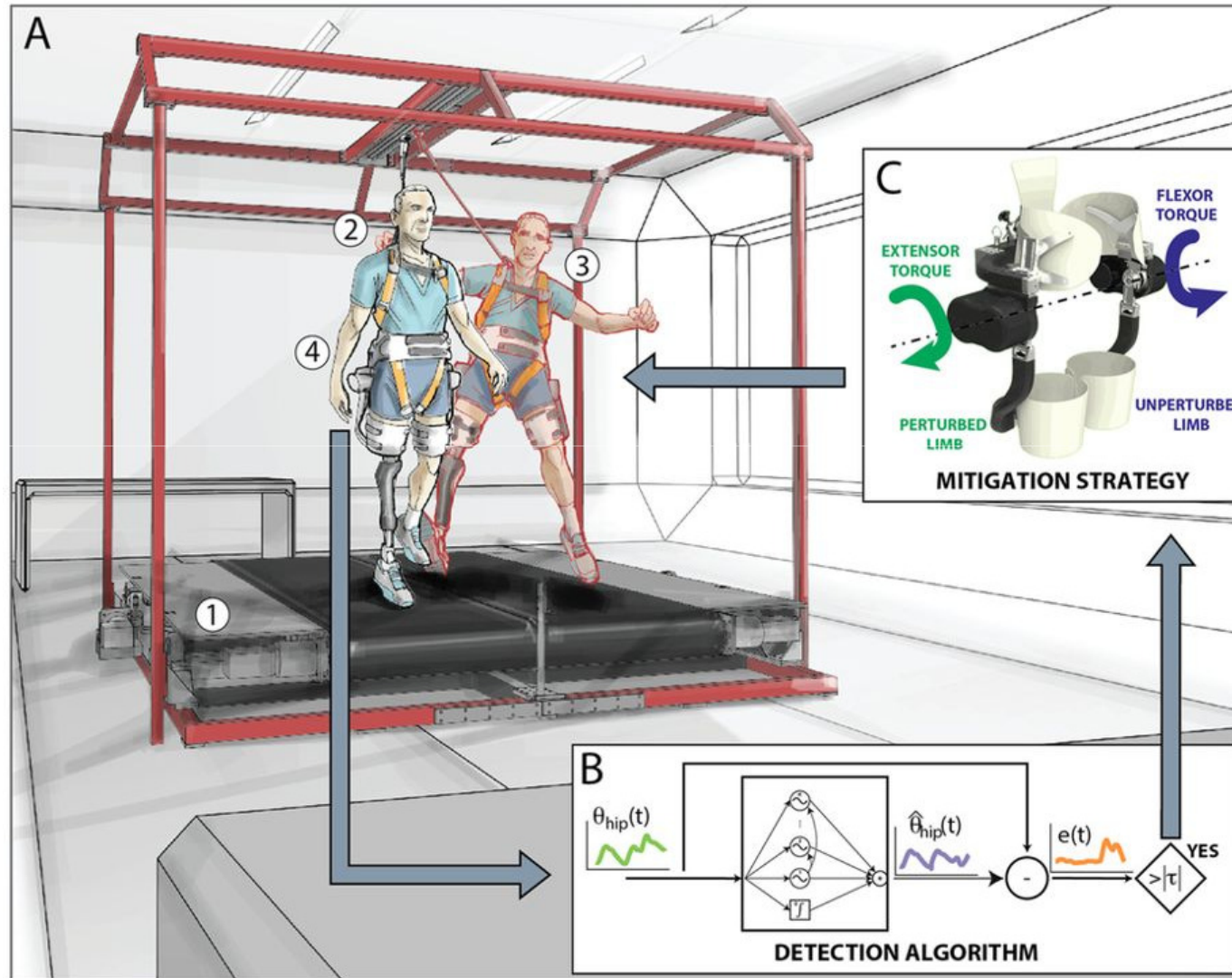
IUVO

www.iuvo.company

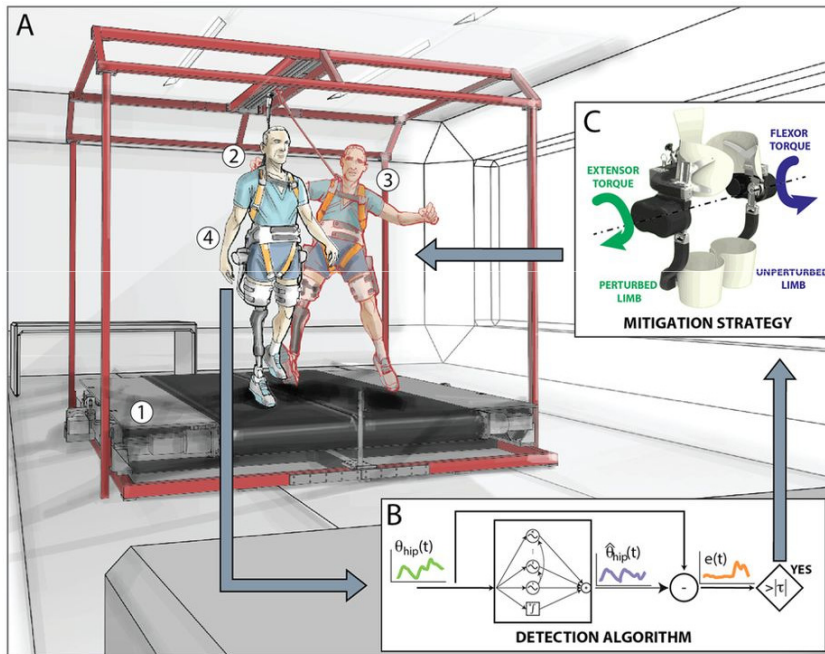
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Overview of the proposed strategy



Overview of the proposed strategy

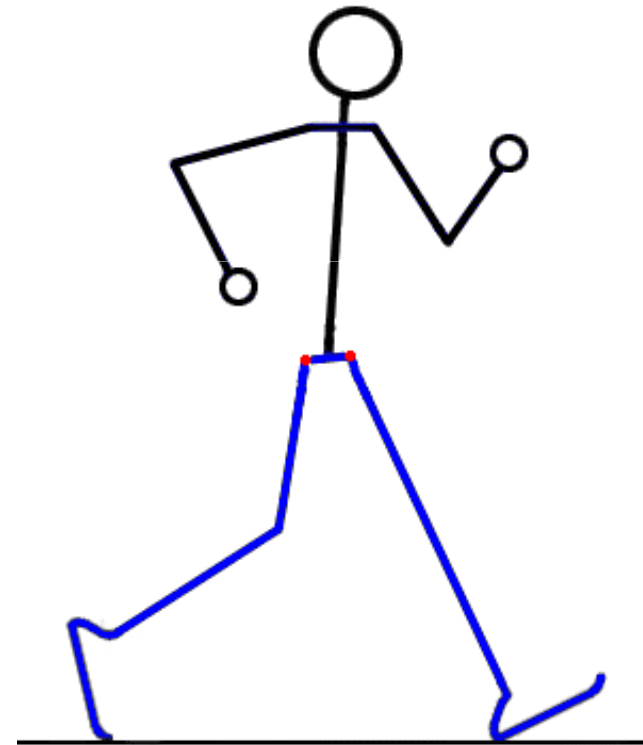
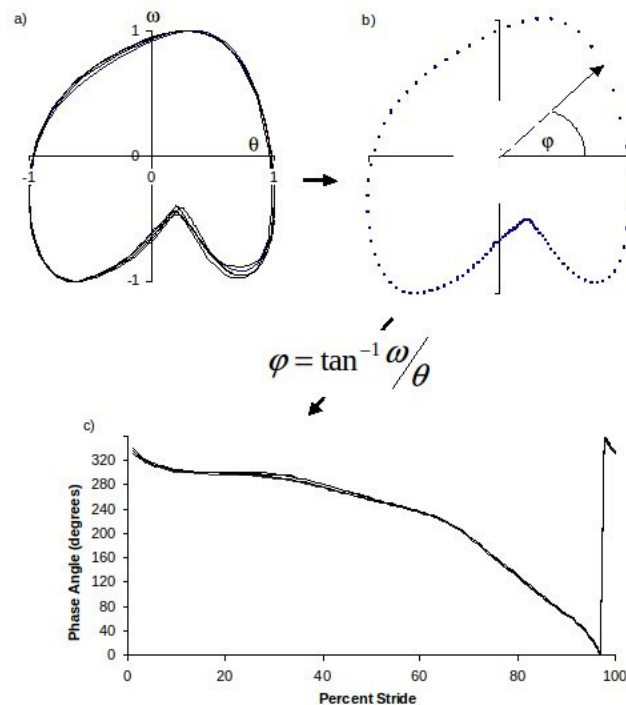


Main issues:

1. Detecting the lack of balance
 - How to do
 - Is it feasible?
 - Is it “on time”?
2. Counteracting the lack of balance
 - How to do
 - Is it effective?
3. Any other approach?

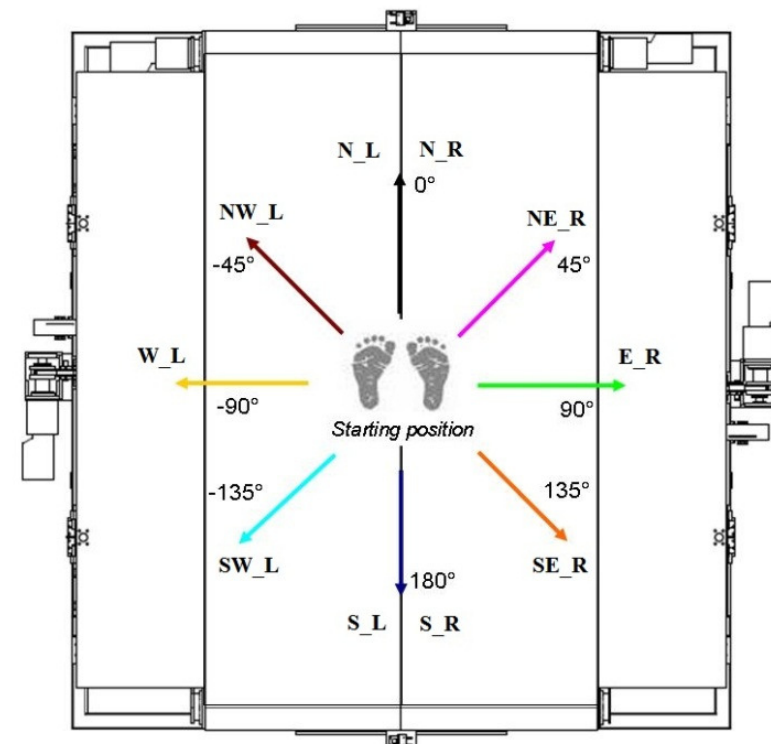
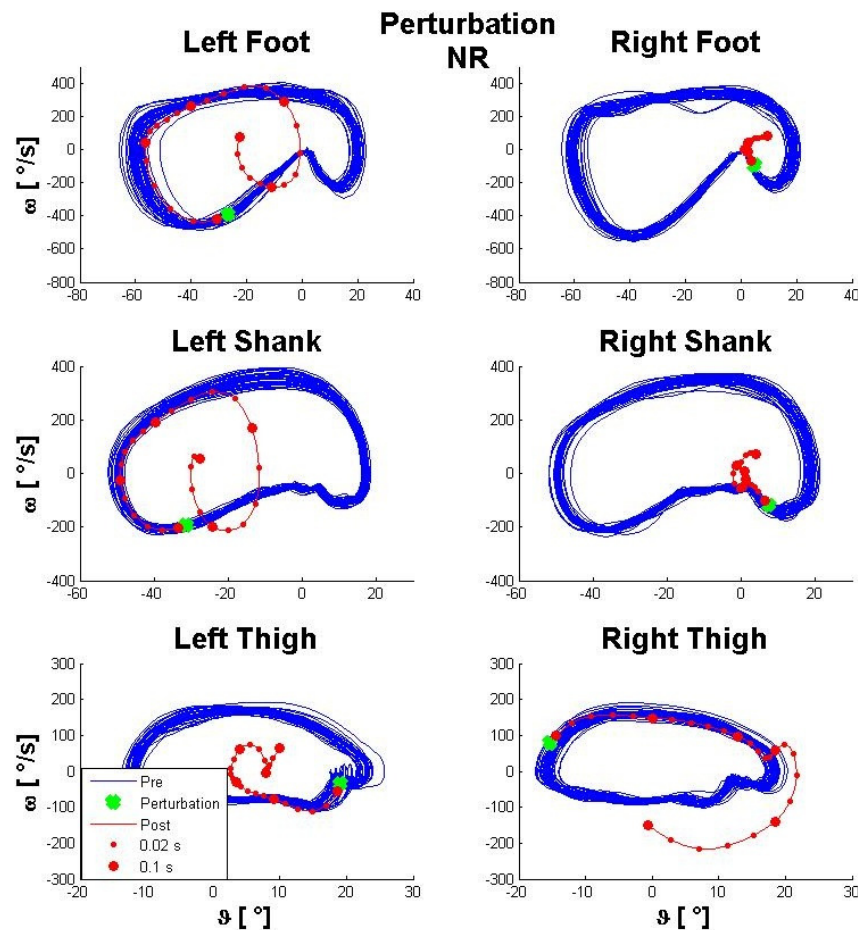
Detecting the lack of balance

Human walking can be considered a quasi automatic and periodic motor task whose features can be described by suitable attractors and/or limit cycles reflecting strong intra-limb and inter-limbs coordination

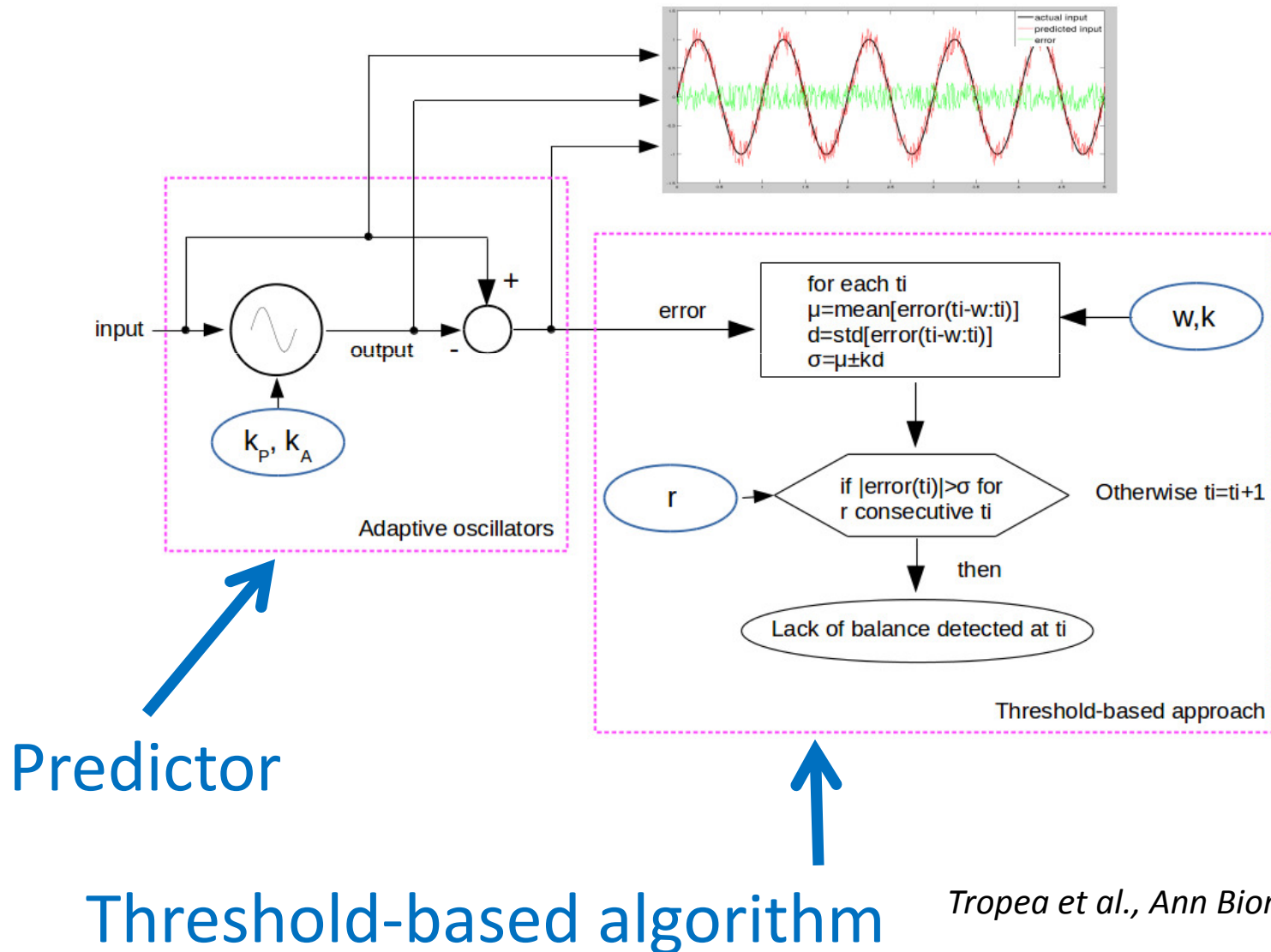


Detecting the lack of balance

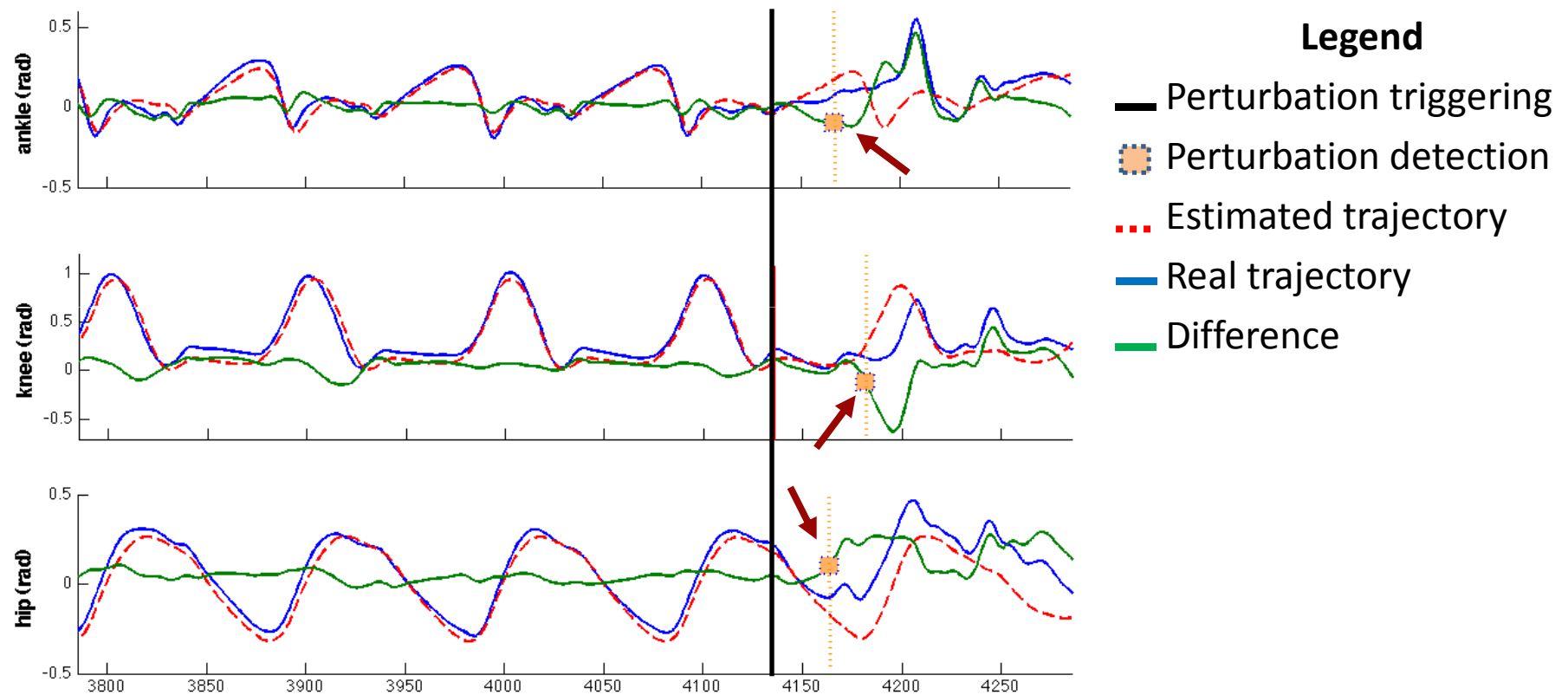
When the dynamics of the locomotion is altered by a sudden and unexpected perturbation, intra- and inter-limbs coordination is modified and their rhythmic features are lost



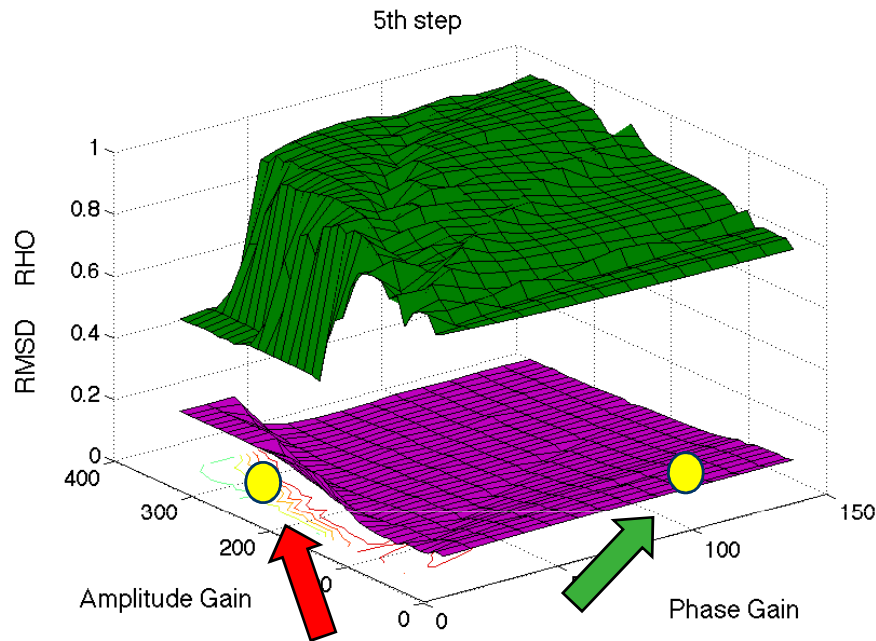
Detecting the lack of balance



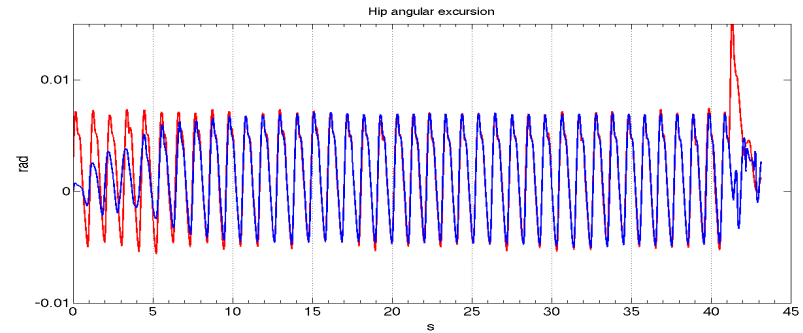
Detecting the lack of balance



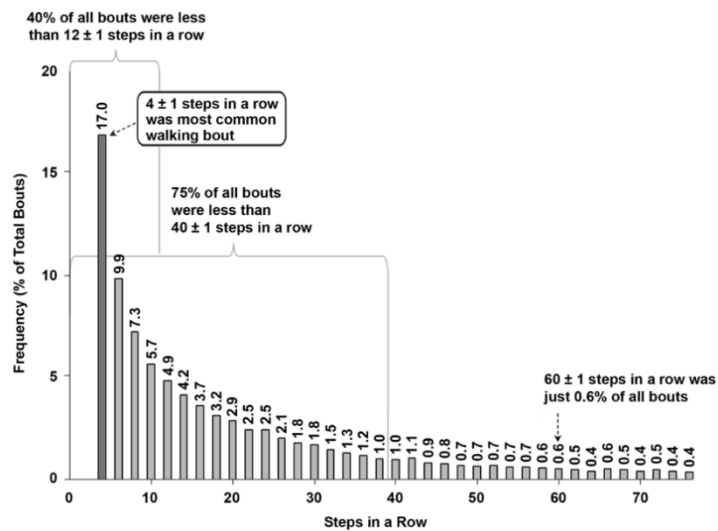
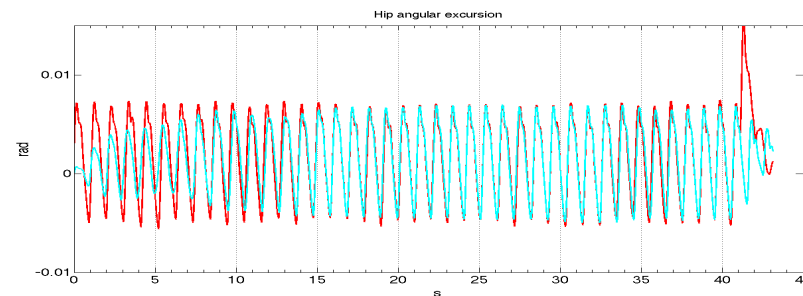
Detecting the lack of balance



GOOD



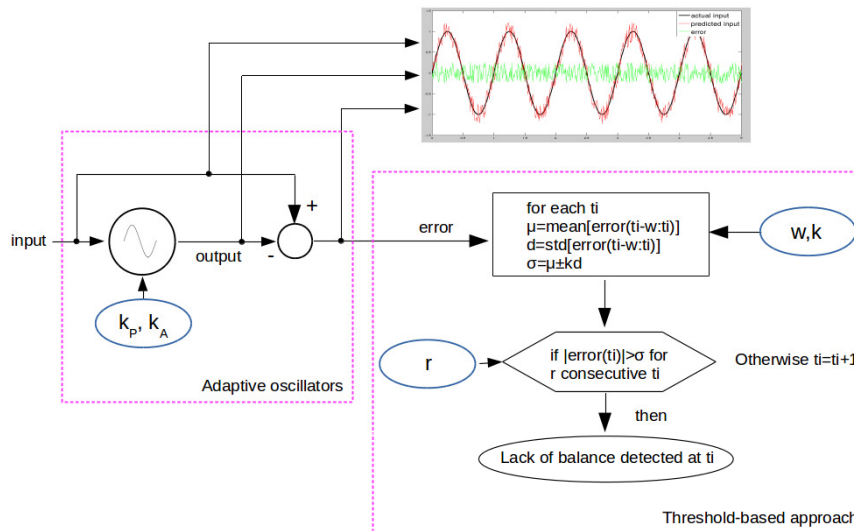
BAD



Tropea et al., Ann Biom Eng 2014

Orenduff et al., JRRD 2008

Detecting the lack of balance

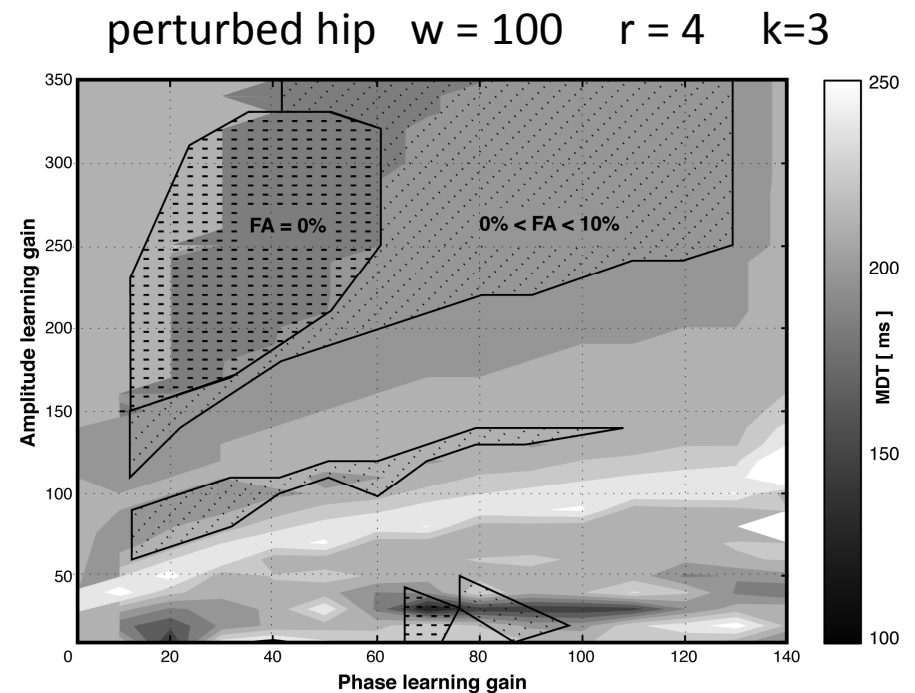


Tuning parameters:

- k_A and k_p , amplitude and phase gains
- w , bin length
- $k\sigma$, threshold
- r , # warning

Optimal tuning:

- min detection time
- min false alarms
- short transitory (4/5 strides)



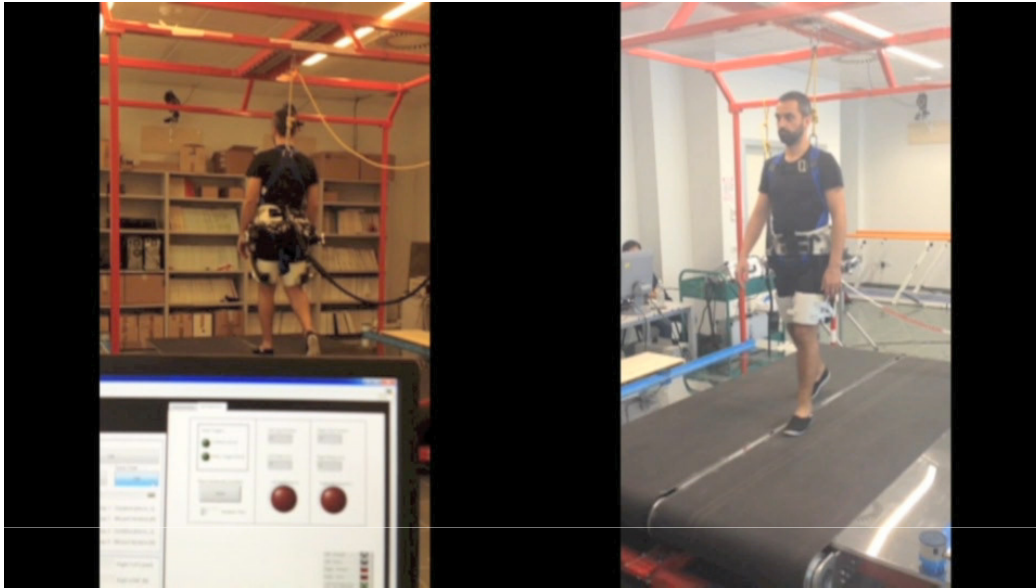
Detecting the lack of balance

Results

Best adaptive oscillator performances

Hip joint angular excursion			
Protocol	Accuracy [%]	Value [ms]	Strides
HS	91.7	289 ± 81	5
TO	88.2	166 ± 12	5

Detecting the lack of balance

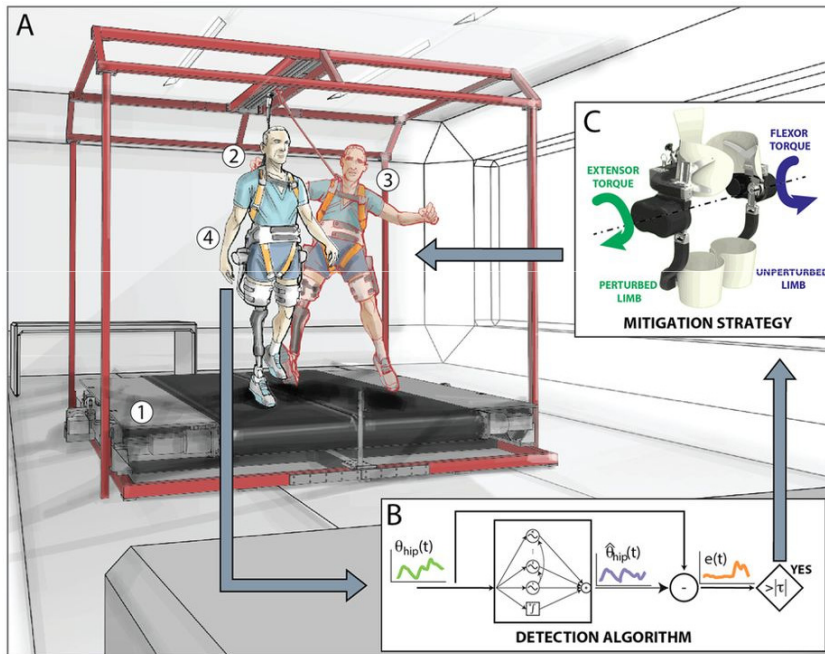


WLK Speed = 1.1 m/s
MDT = 291 ms





WLK Speed = 0.64 m/s
MDT = 403 ms

Overview of the proposed strategy



Main issues:

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2. Counteracting the lack of balance

- How to do
- Is it effective?

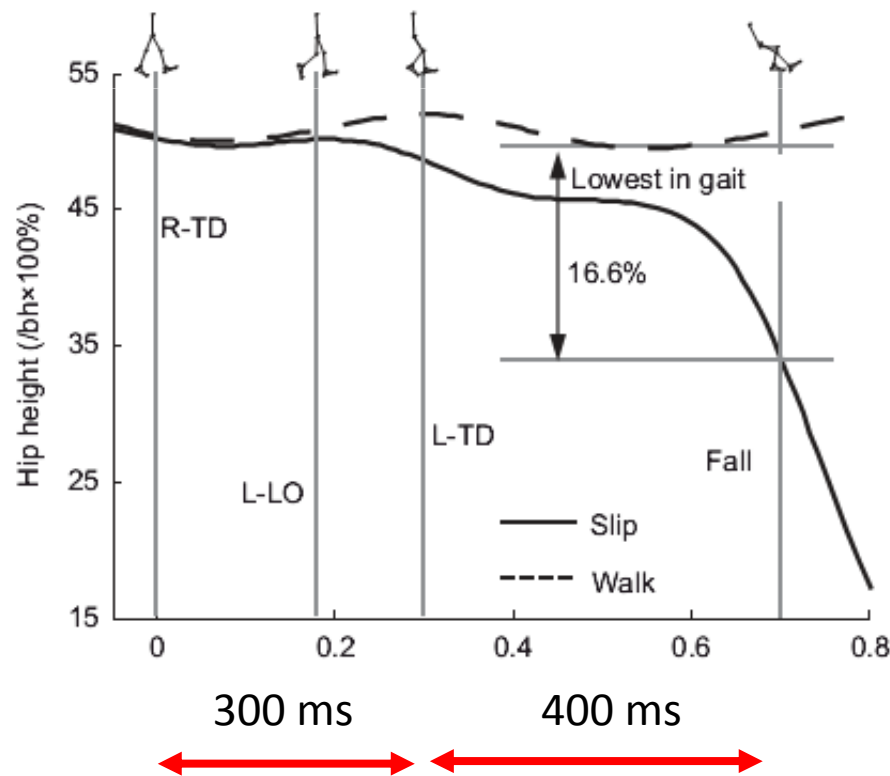
3. Any other approach?

Detecting the lack of balance



Role of stability and limb support in recovery against a fall following a novel slip induced in different daily activities

Feng Yang, Tanvi Bhatt, Yi-Chung Pai*

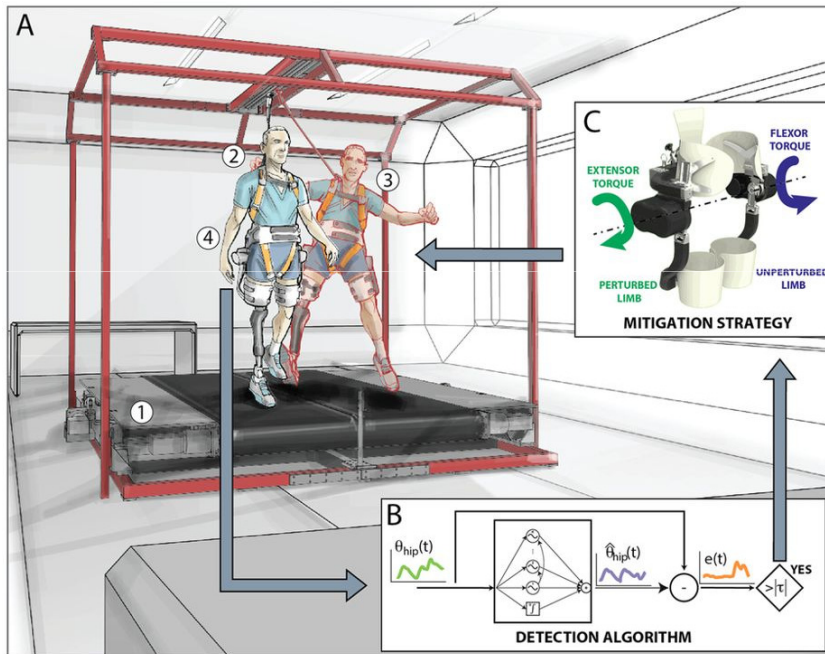


After about 300-400 ms, the lack of balance not longer recoverable and turns to fall

Q. Are we on time?




A. Yes, just in time (fortunately)

Overview of the proposed strategy



Main issues:

1. Detecting the lack of balance

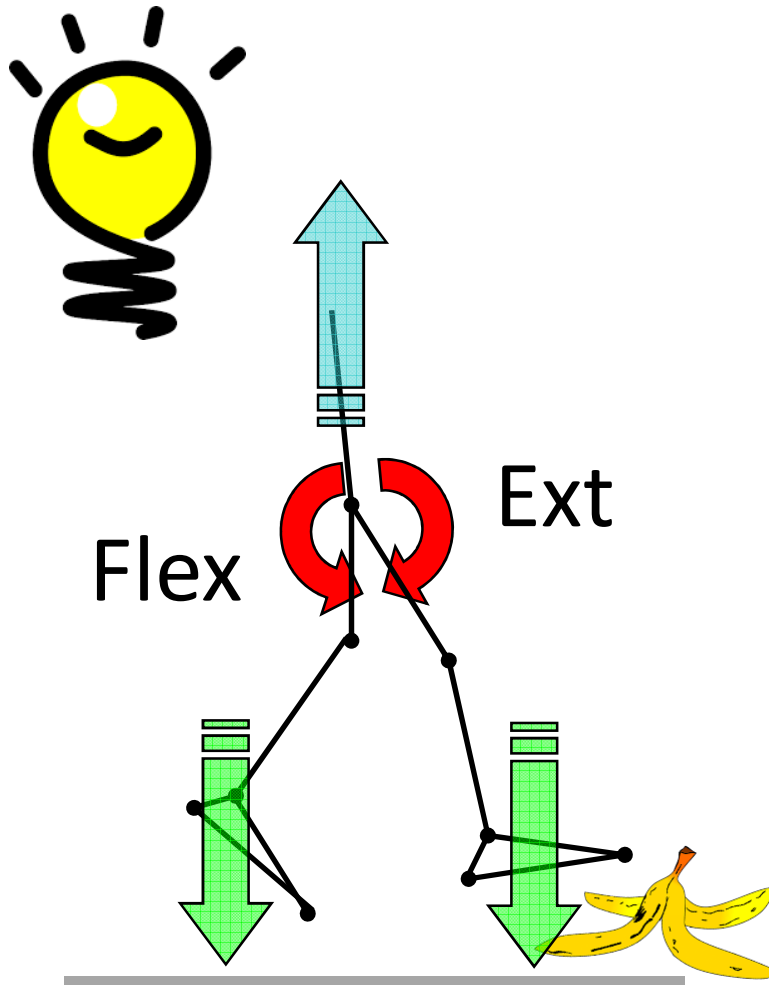
- How to do 
- Is it feasible? 
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2. Counteracting the lack of balance

- How to do
- Is it effective?

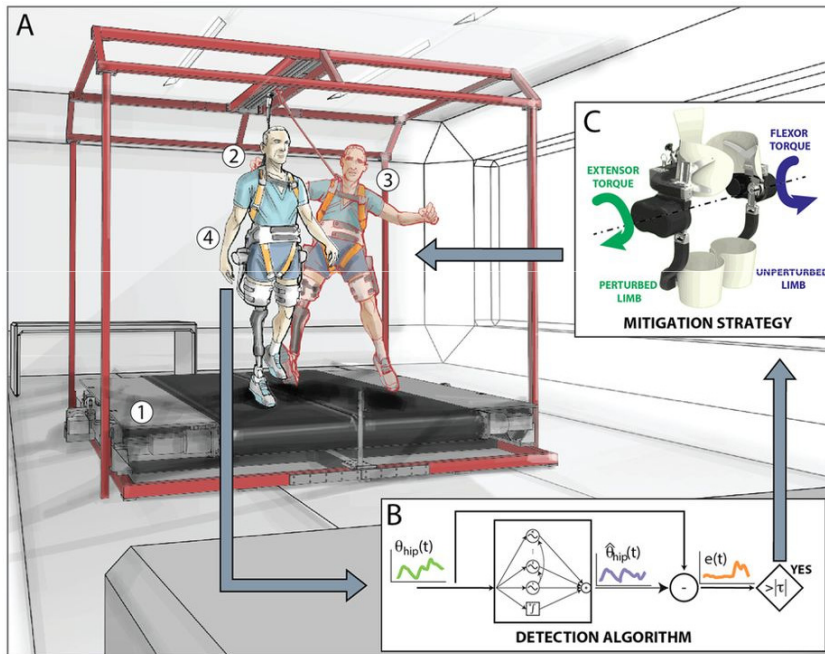
3. Any other approach?

Counteracting the lack of balance






1. The forward foot starts slipping
2. The algorithm detects the lack of balance [350 ms]
3. The APO acts on the hips
 - Torque $0.2 \times BW$ [empirical]
 - To increase the foot-ground interaction
 - To push upward the CoM

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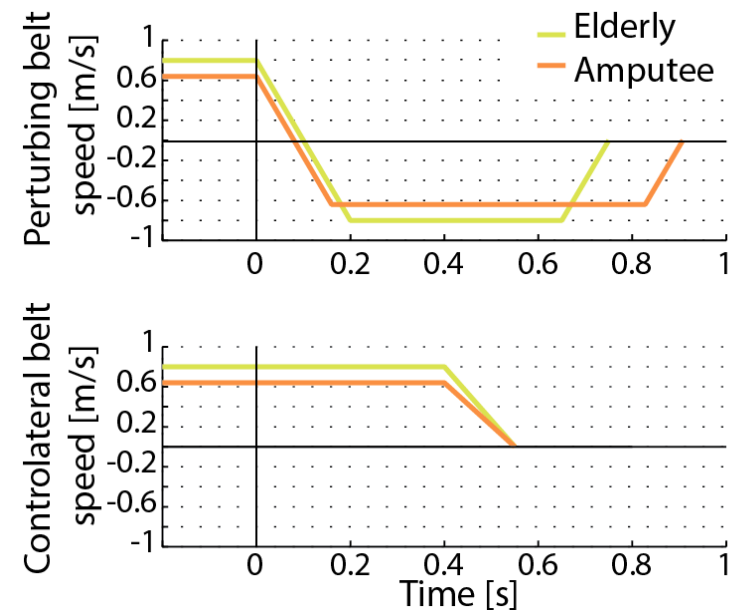
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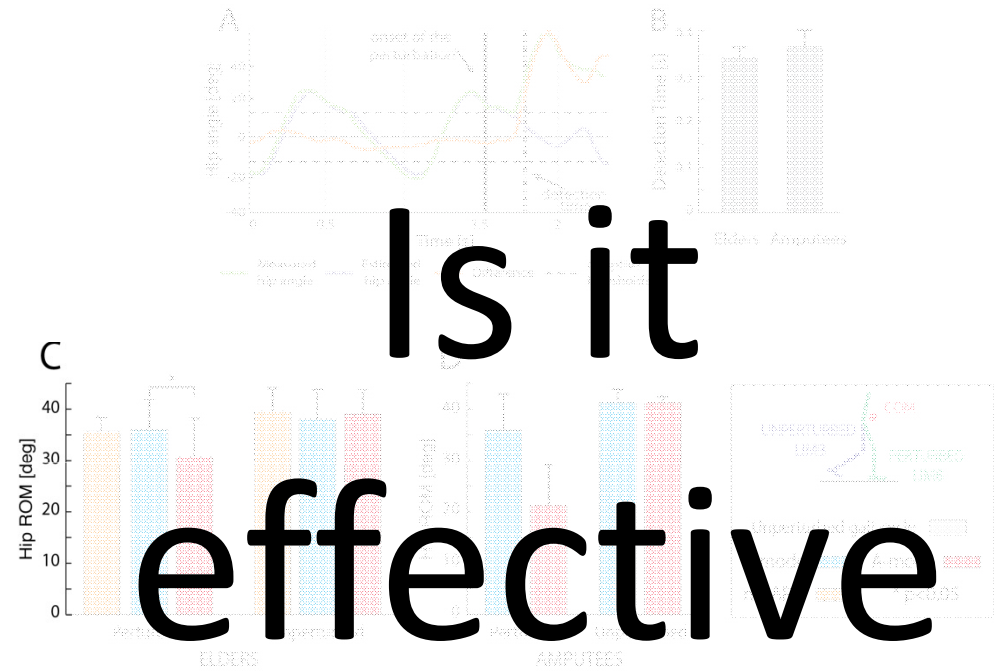
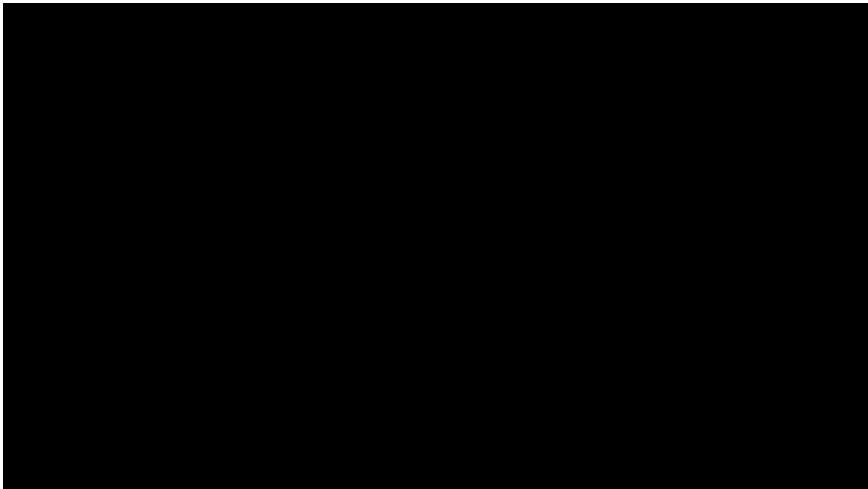
3. Any other approach?

Materials and Methods

- Participants
 - 8 older adults (males, 69.9 ± 5.1 ys)
 - 2 transfemoral amputees (age- and anthropometry- matched)
 - no other comorbidities
- Walking speed: self selected
 - elders: 0.89 ± 0.11 m/s
 - amputees: 0.69 ± 0.06 m/s
- Perturbation: unexpected slippage
 - elders: right foot
 - amputees: **prosthetic foot**
- Whole body 3D kinematics (34 MRKs)
- APO
 - Z – Mode \rightarrow transparent
 - A – Mode \rightarrow assistive

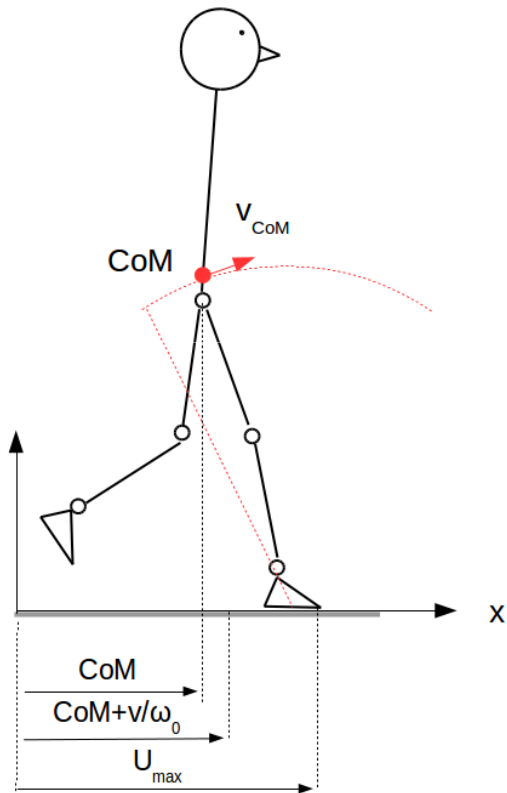


Counteracting the lack of balance



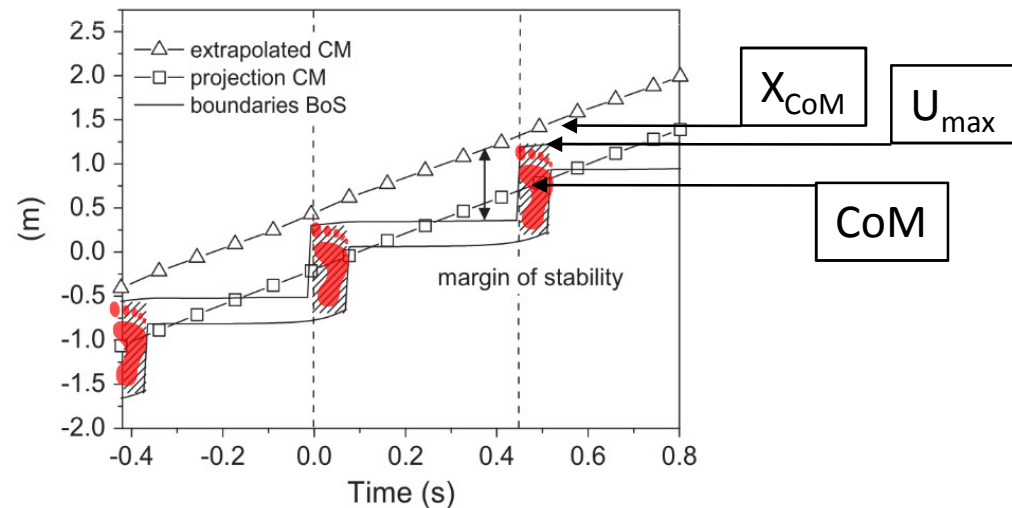
- Is it effective?
- Detection Algorithm ON TIME
 - Faster bipodal support
 - Lower num. of recovering steps
 - Modification of hip joint angle

Assessing the Stability: CoM vs BoS Margin of Stability



$$MoS = U_{max} - \left(CoM - \frac{v_{CoM}}{\omega_0} \right) = U_{max} - X_{CoM}$$

$$\omega_0 = \sqrt{g/h_{CoM}}$$

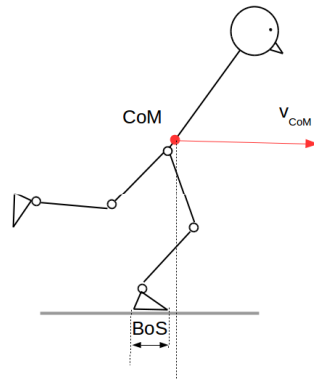
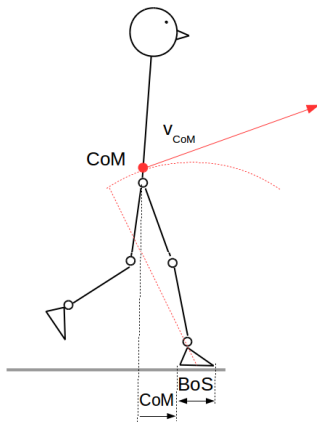


MoS < 0 [slightly] ---> controllable lack of balance

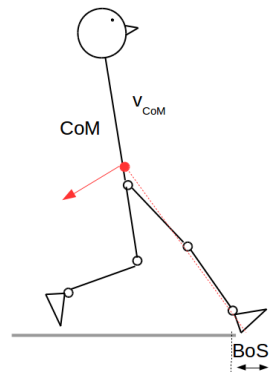
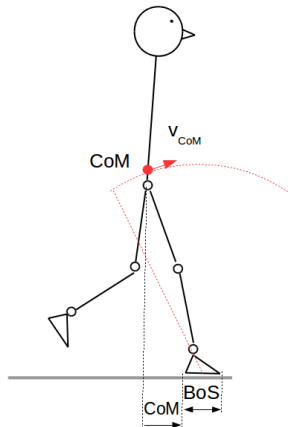
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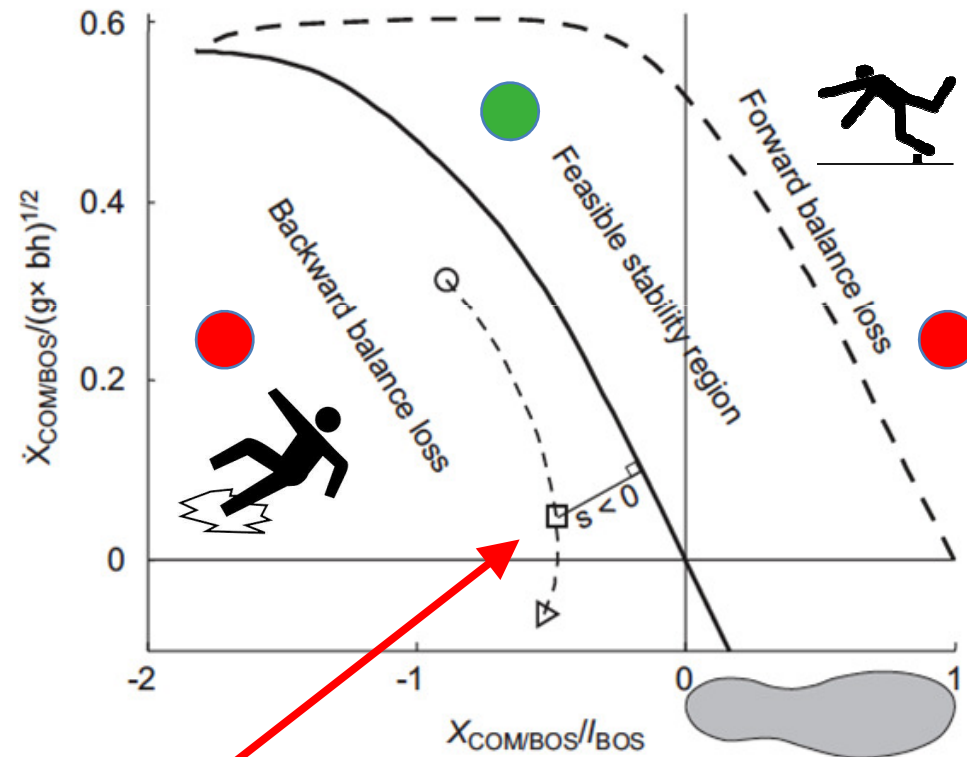
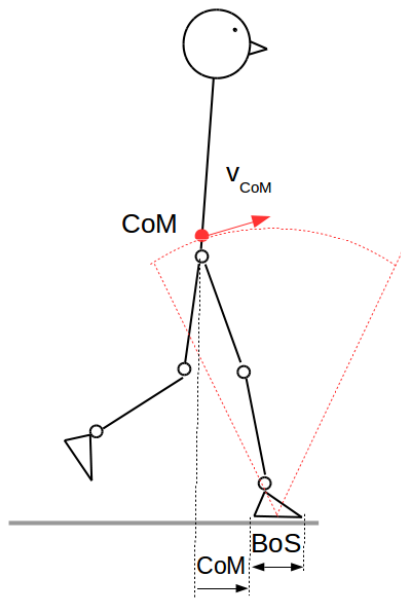
MoS << 0 ---> FORWARD fall



MoS >> 0 ---> BACKWARD fall

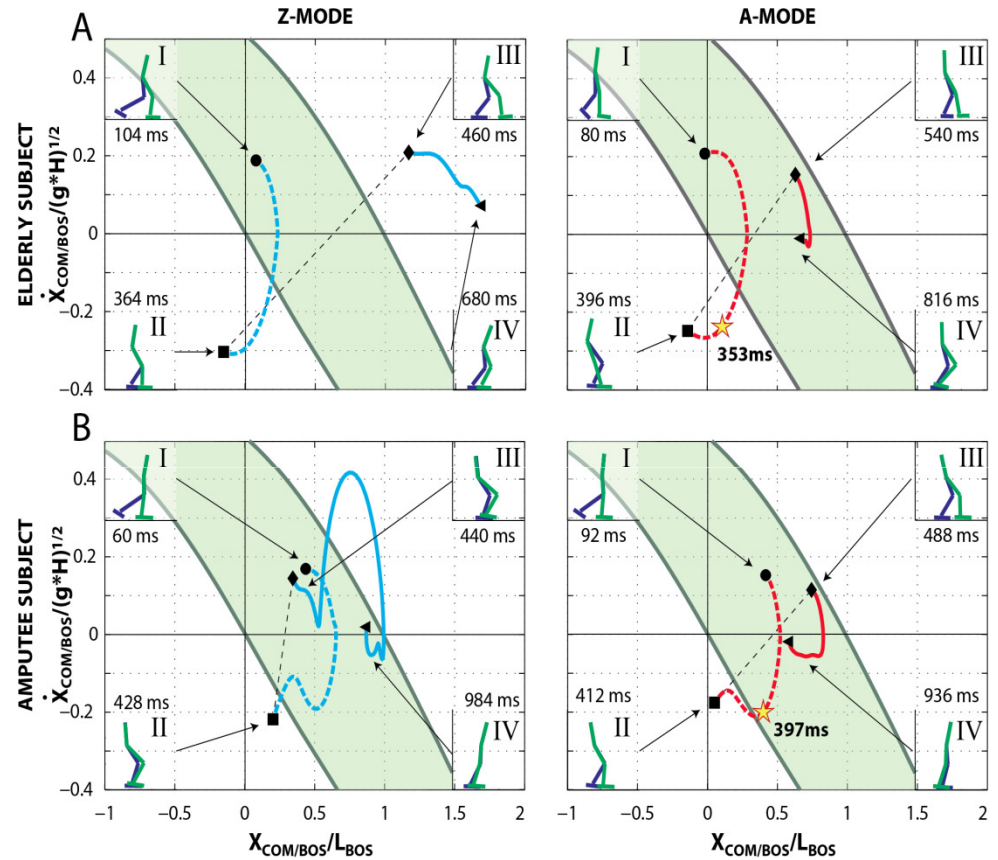
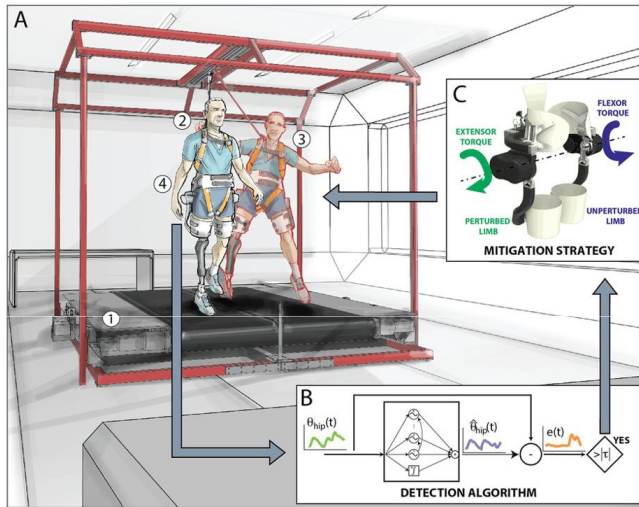
Assessing the Stability: CoM vs BoS

CoM Stability

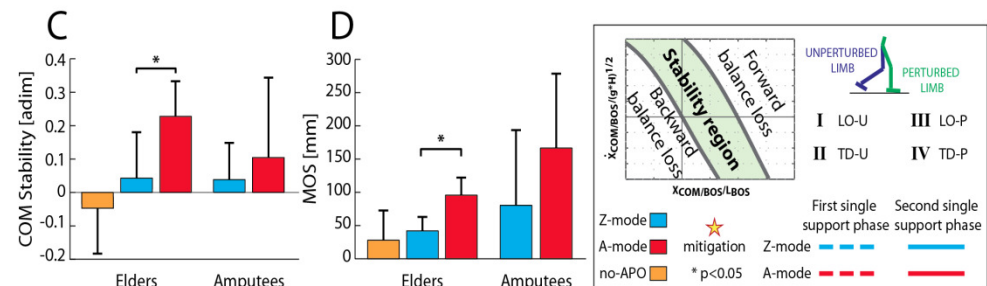


CoM stability

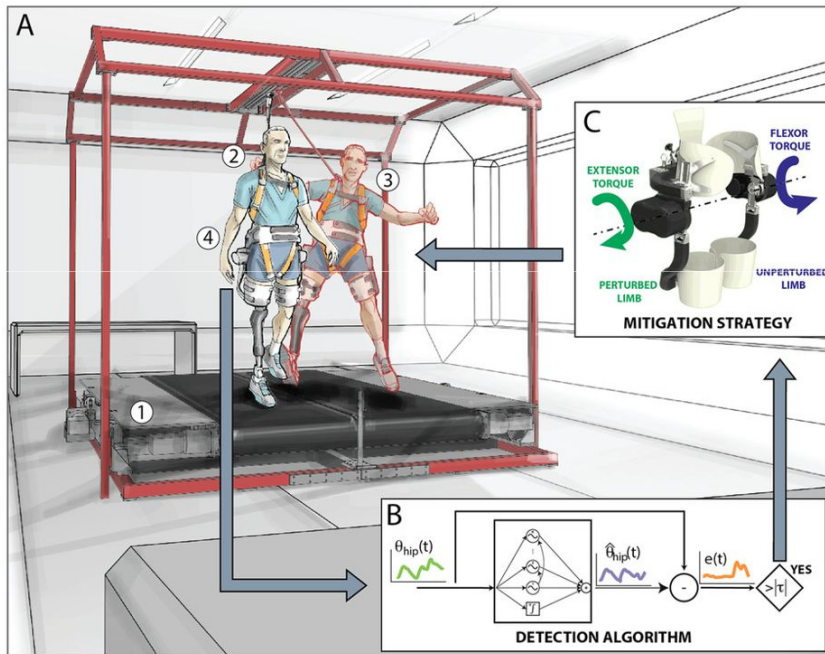
Counteracting the lack of balance: is it effective?



Yes, it is!






Overview of the proposed strategy





Main issues:

1. Detecting the lack of balance

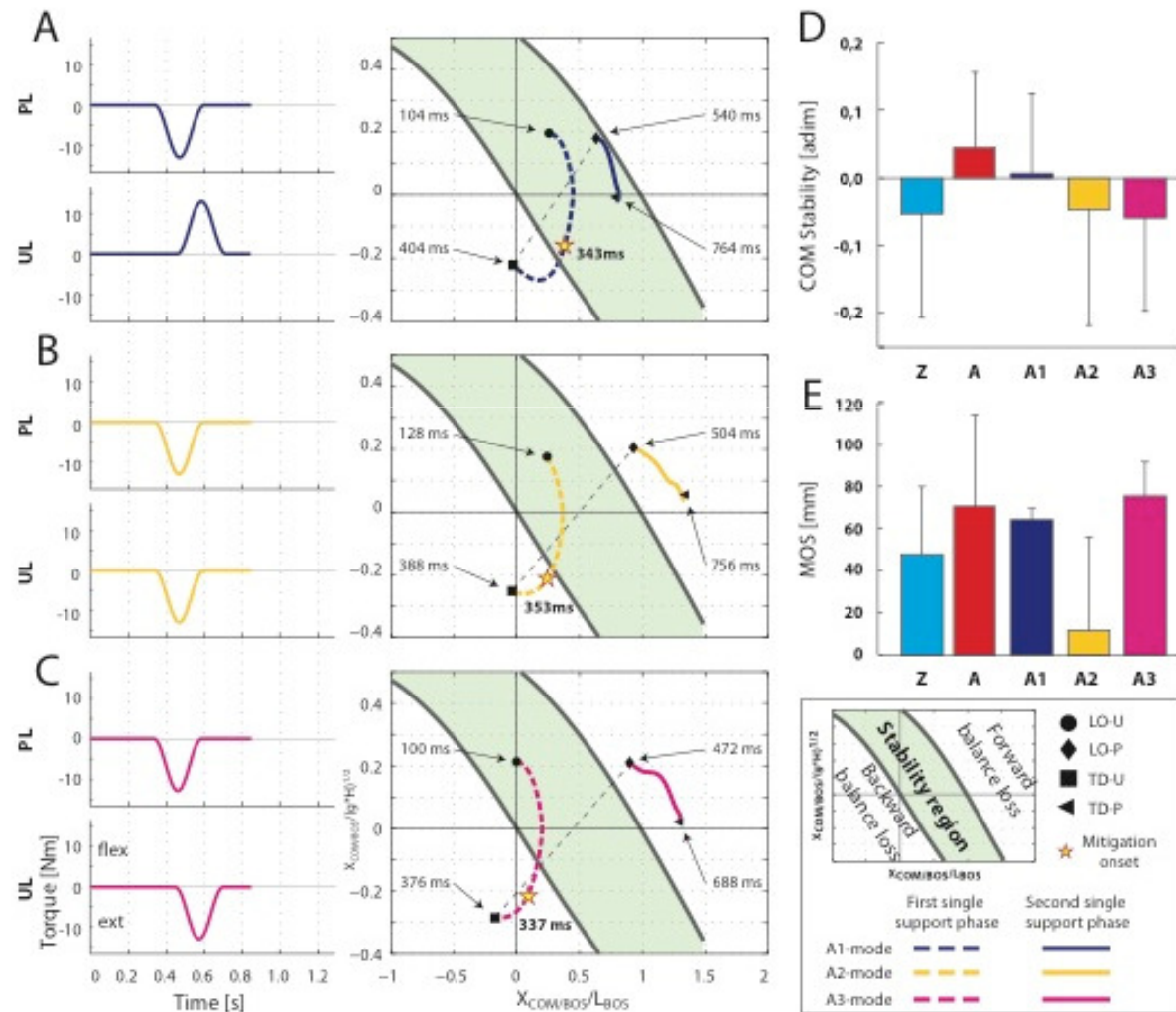
- How to do 
- Is it feasible? 
- Is it “on time”? 

2. Counteracting the lack of balance

- How to do 
- Is it effective? 

3. Any other approach?

Counteracting the lack of balance: alternative strategies



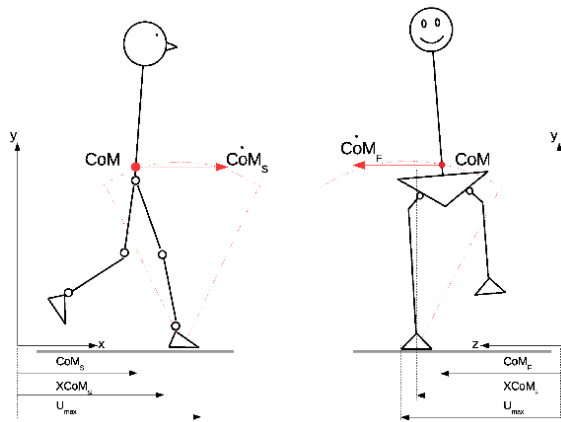
Outline of the presentation

- Fall risk: what are we talking about?
- State of art
 - Assessing the fall risk
 - Detecting falls/lack or balance
 - Counteracting falls/lack of balance
- Wearable robot: the dream
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 - SENLY
 - Active Pelvis Orthosis
- A possible strategy
 - Detection Algorithm
 - Assistive strategy
- **Ongoing activities**
 - **Different perturbations**
 - **Other approaches for the detection**
 - **Robotic prosthesis**
- Conclusions

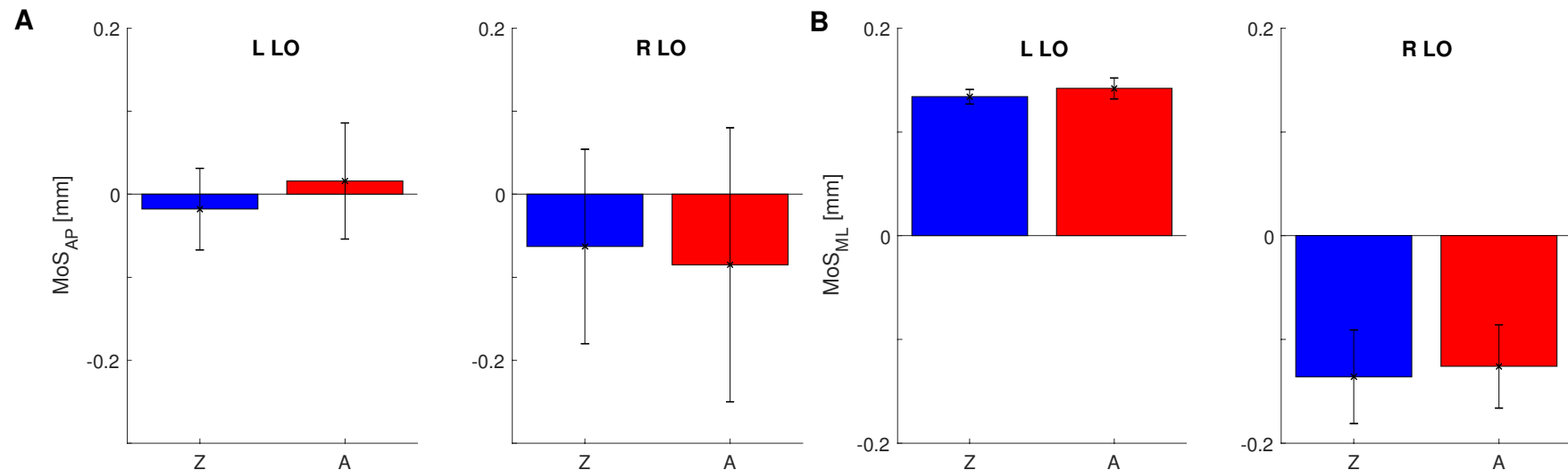
Is the proposed strategy effective after multi-directional slippages?



Is the proposed strategy effective after multi-directional slippages?



No differences between **Z-mode (no assistance)** and **A-mode (with assistance)**

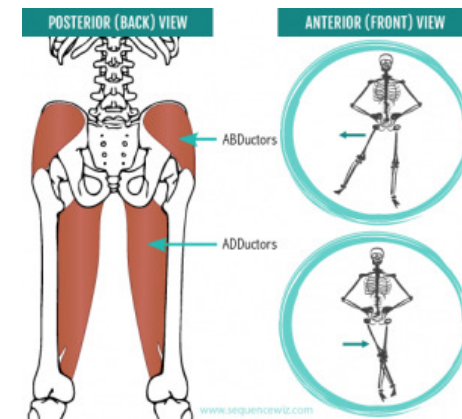


Is the proposed strategy effective after multi-directional slippages?

On, it is not effective! Why?

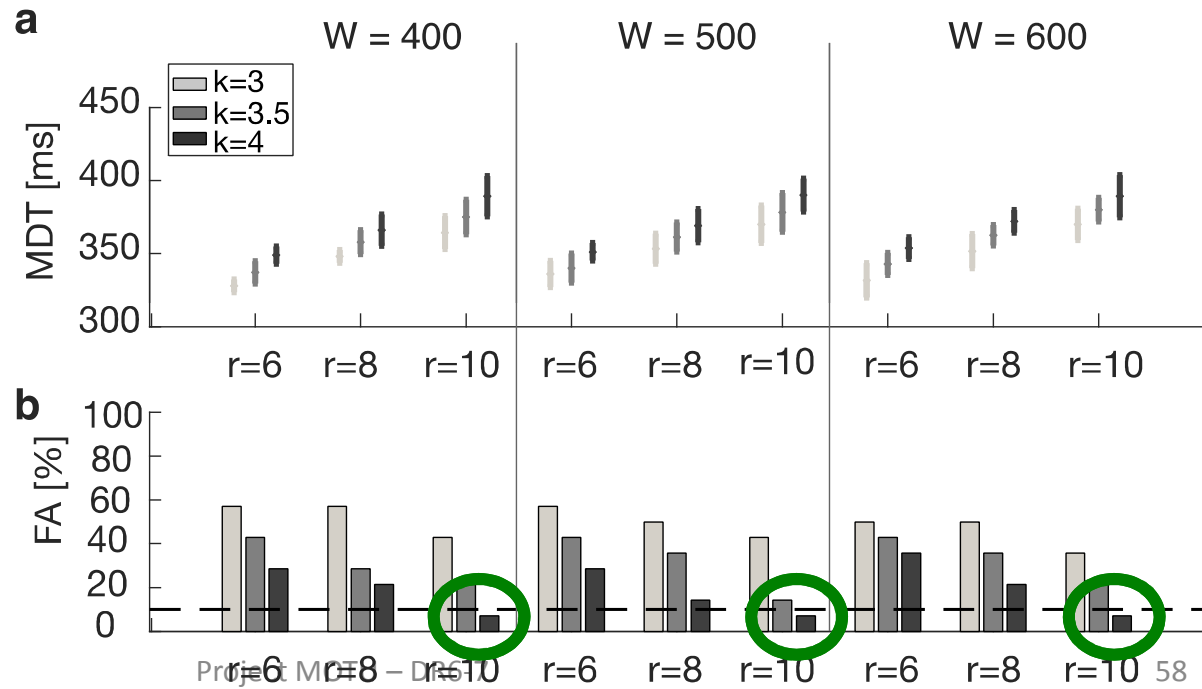
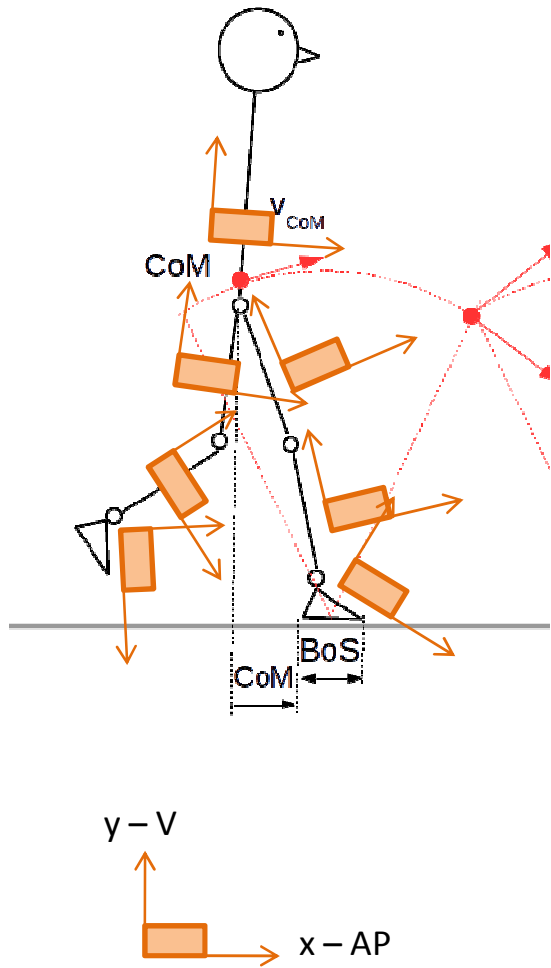
- ▶ MDT > 450 ms (too high)
- ▶ CLs APO cannot measure and control hip ab/adduction

Tuning parameters					ML slippages	
k_p	k_a	w	r	k	MDT [ms]	FA [%]
40	1	900	6	3.5	455±35	57
10	1	1000	10	3.5	467±21	79
40	1	1000	6	3.5	461±36	50

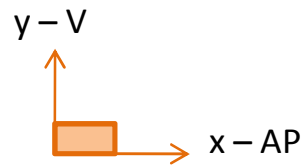
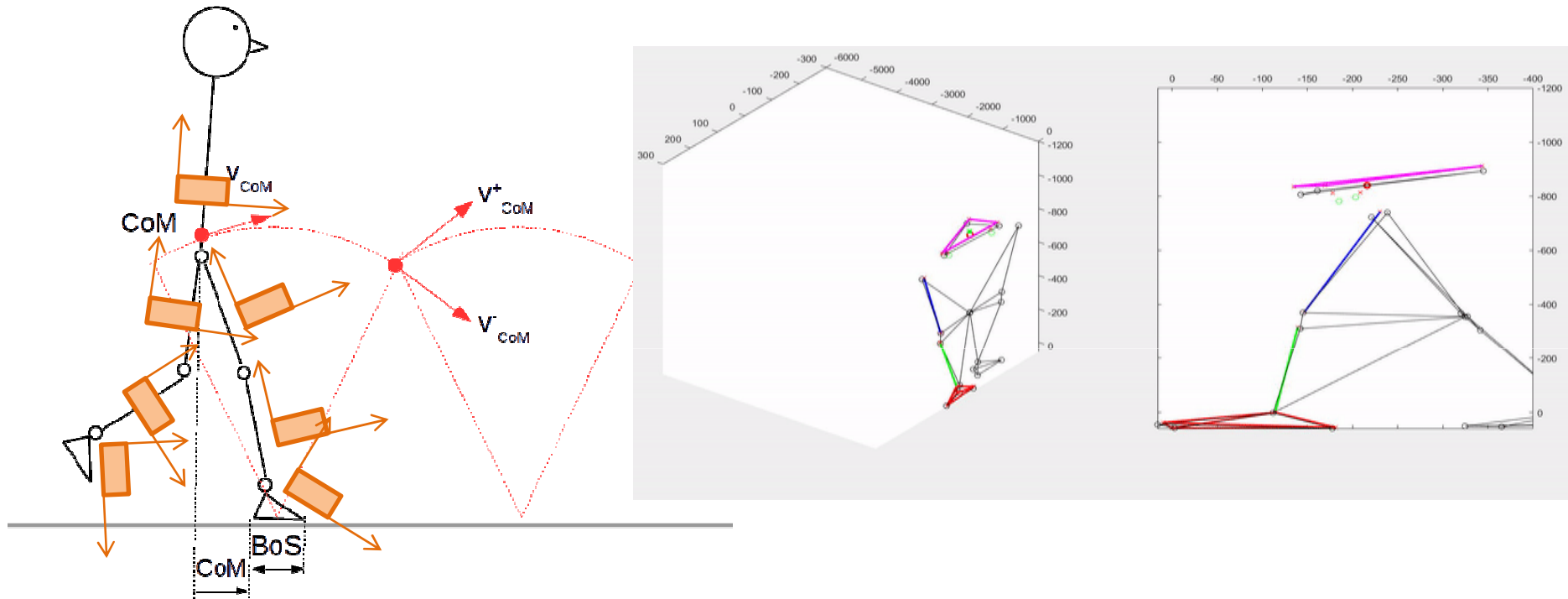


What about using IMUs?

Detecting slippages

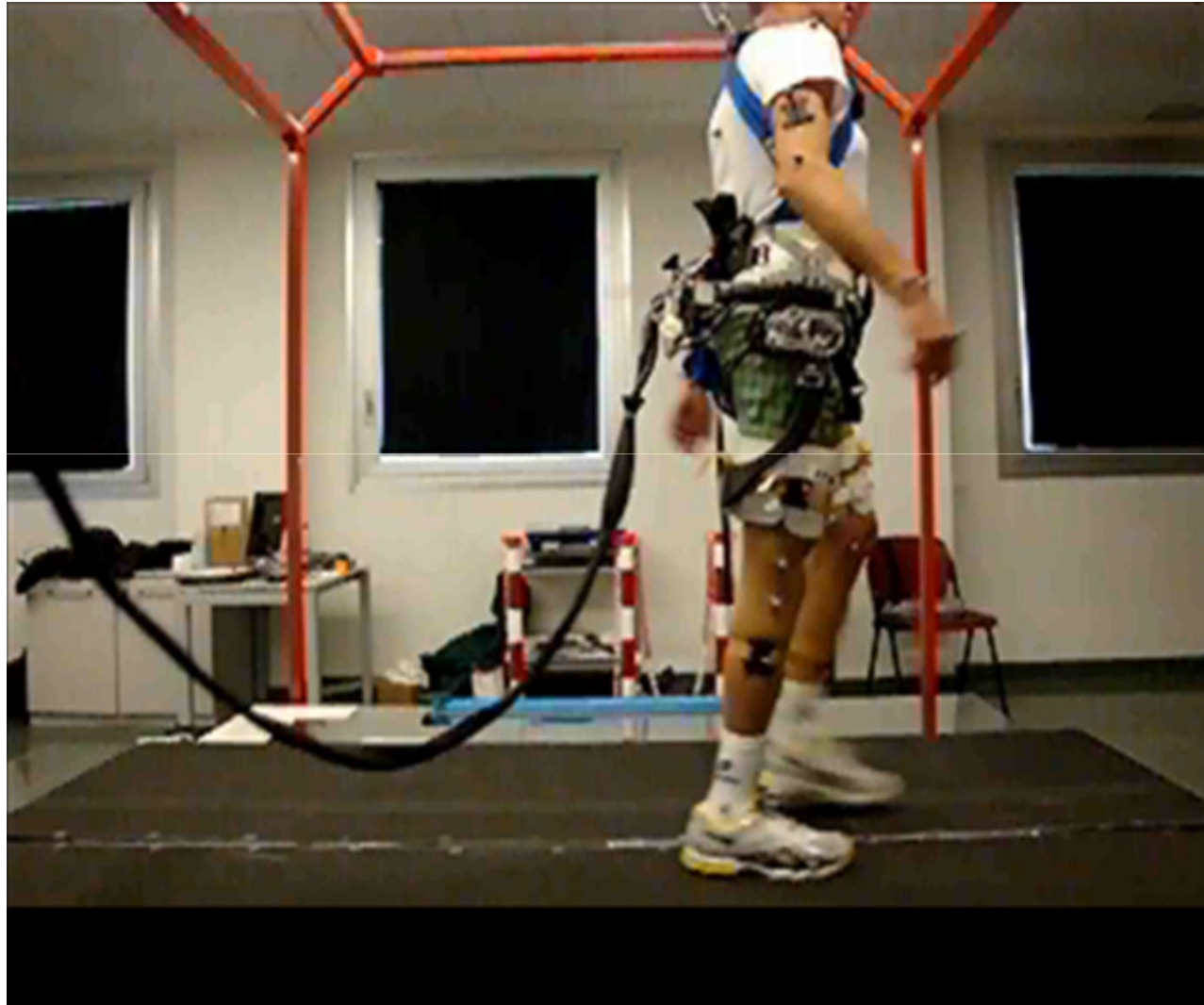


What about using IMUs?



Q. Can we estimate the MOS at run time?
A. Yes, we can!

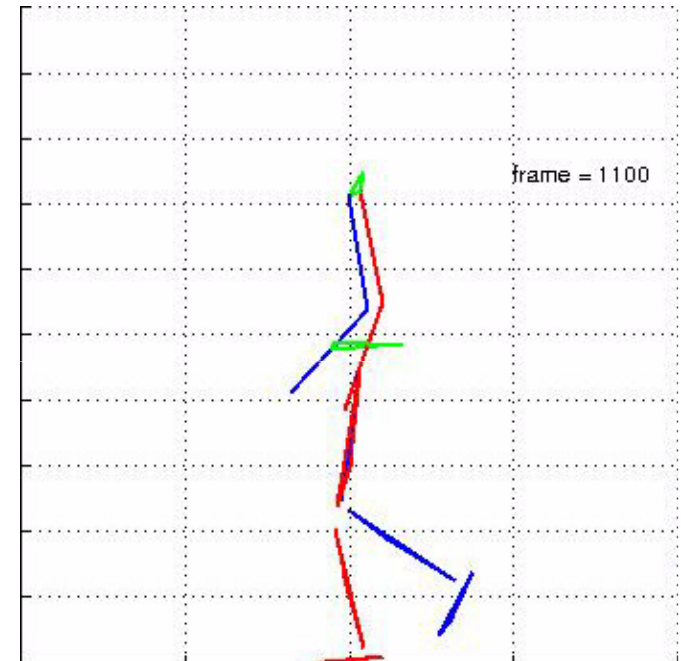
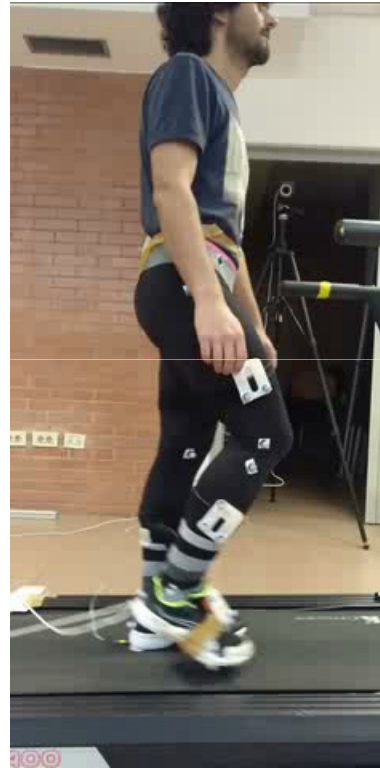
Robotic prosthesis



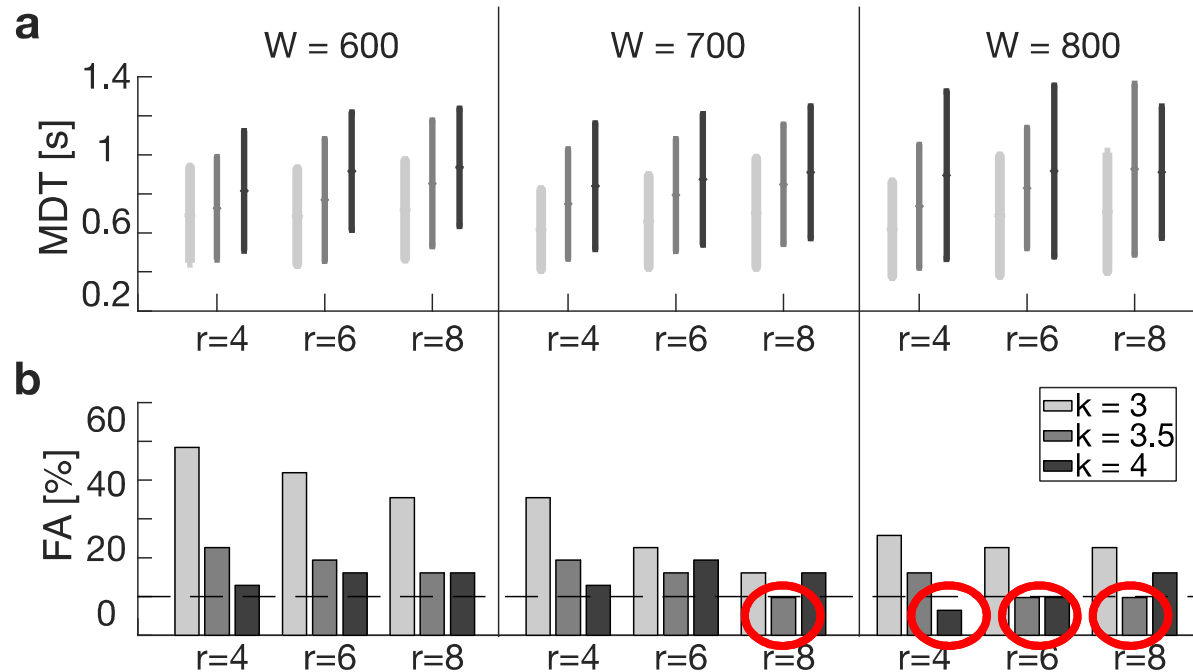
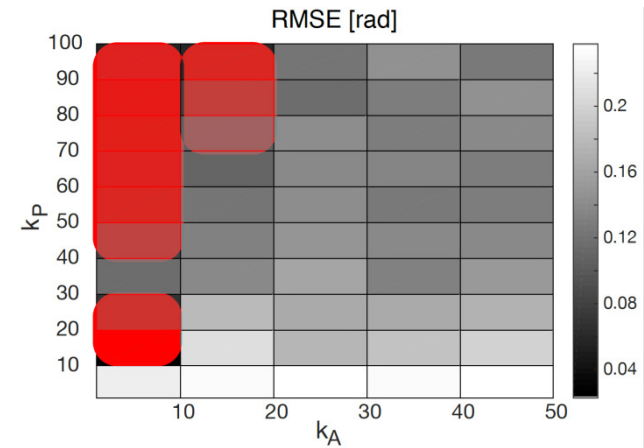
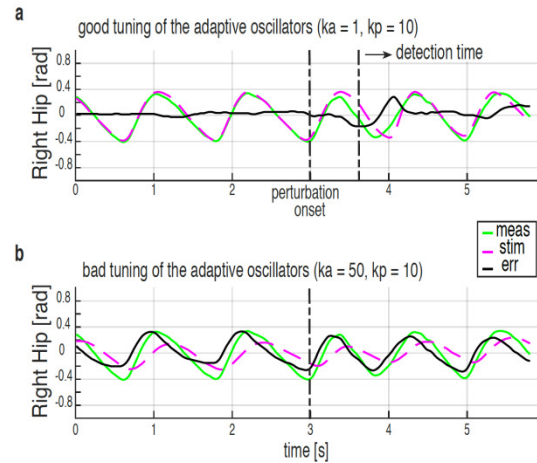
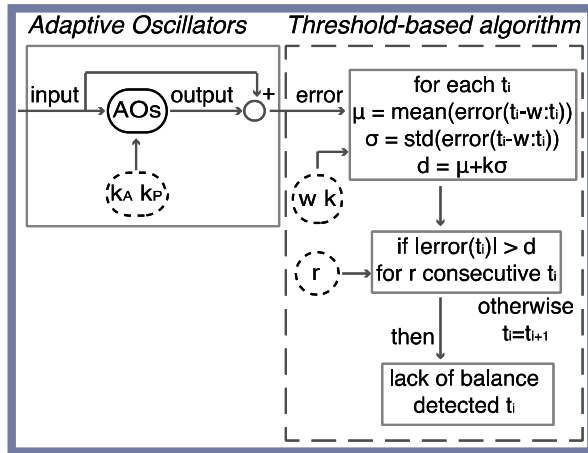
Tripping



1. perturbed foot; 2. spring-rope mechanisms; 3. treadmill; 4. footswitch under the unperturbed foot; 5. cam-based braking mechanisms.



Tripping: detection based on HIP

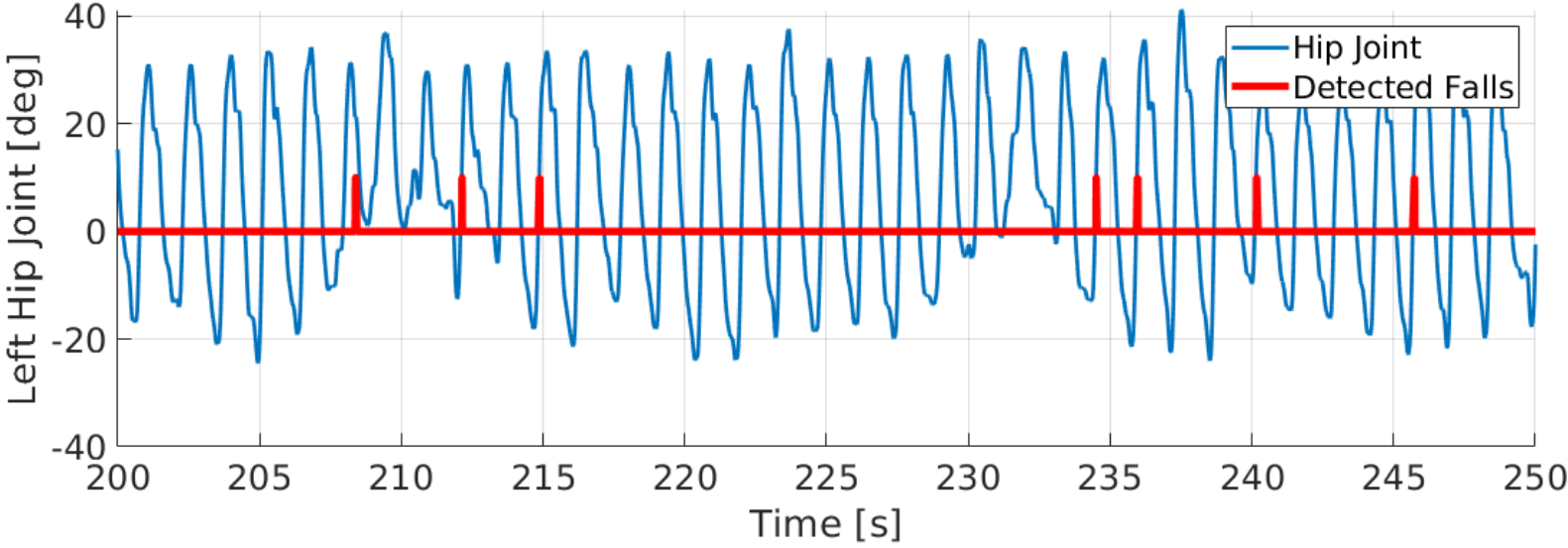
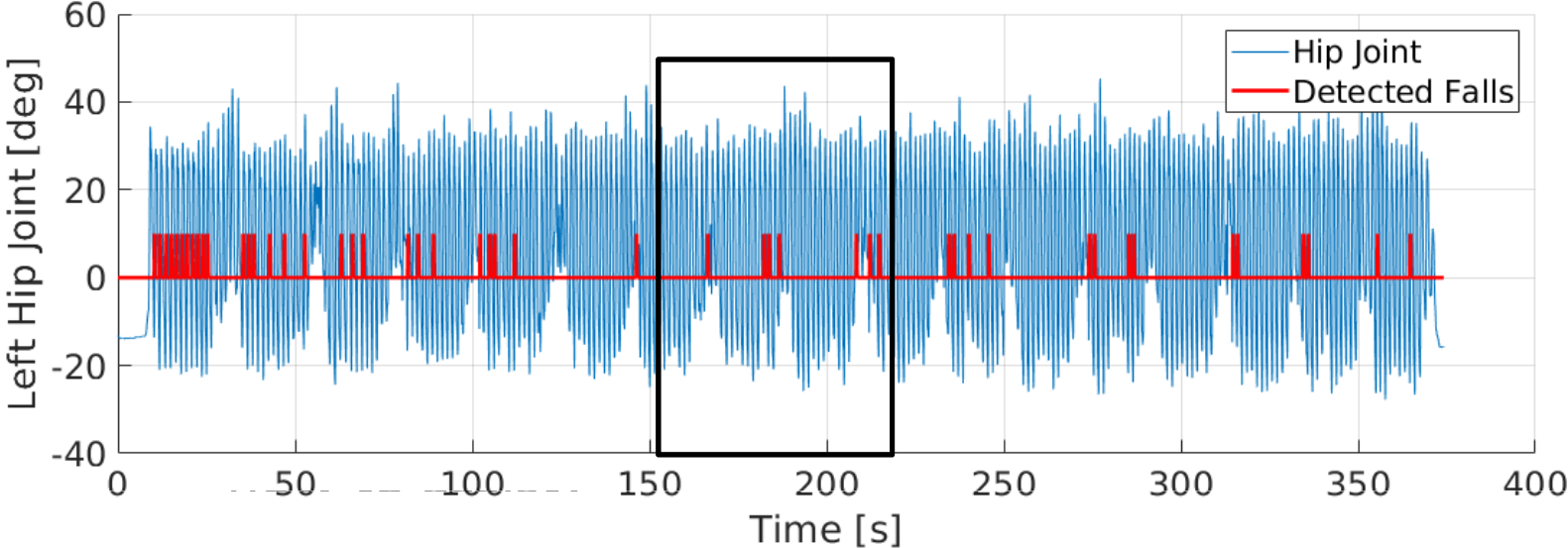


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Conclusions (1/3)

LEFT SIDE



Conclusions (2/3)

Q. Can we generalize the proposed strategy to different perturbations (e.g., tripping, obstacle avoidance)?

A1. The “detection” procedure can be easily generalized even if tests in ecological conditions are required.

A2. The APO-mediated assistive behavior needs to be investigated

Conclusions (3/3)

Q. Any limit?

A. A bunch of limits!!!

However, we hope to be on the right way.



Acknowledgments (1/2)



S. Micera



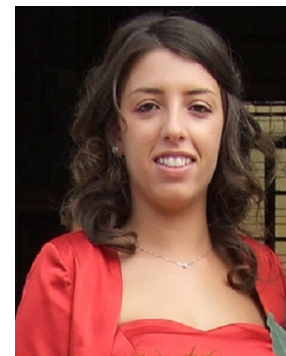
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CYBERLEGs ++

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Acknowledgments (2/2)



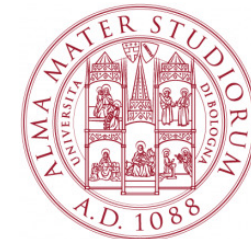
S. Micera



V. Monaco



F. Aprigliano



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Counteracting balance loss by using wearable robotics

Speaker: Vito Monaco

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Bari, 20 May 2019